

A Survey of Compressive Sensing and Applications

Justin Romberg

Georgia Tech, School of ECE

ENS Winter School

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Signal processing trends

DSP: sample first, ask questions later

Explosion in sensor technology/ubiquity has caused two trends:

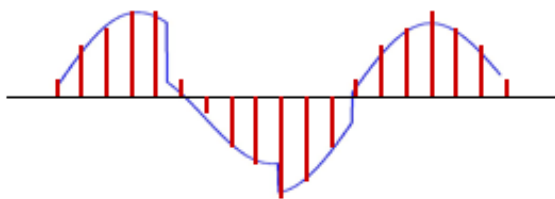
- Physical capabilities of hardware are being stressed, increasing speed/resolution becoming *expensive*
 - ▶ gigahertz+ analog-to-digital conversion
 - ▶ accelerated MRI
 - ▶ industrial imaging
- Deluge of data
 - ▶ camera arrays and networks, multi-view target databases, streaming video...

Compressive Sensing: sample smarter, not faster

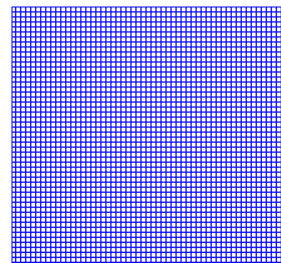
Classical data acquisition



- *Shannon-Nyquist sampling theorem* (Fundamental Theorem of DSP):
“if you sample at twice the bandwidth, you can perfectly reconstruct the data”



time



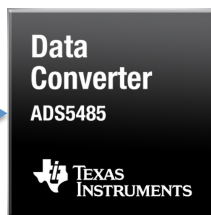
space

- Counterpart for “indirect imaging” (MRI, radar):
Resolution is determined by bandwidth

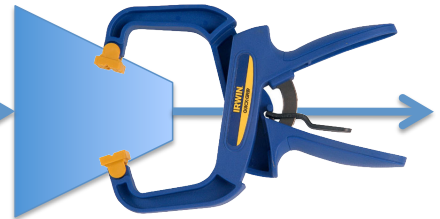
Sense, sample, process...



sensor



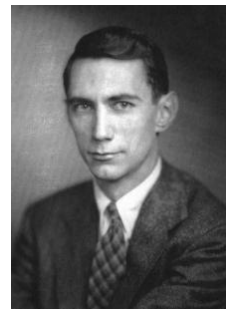
"fast" ADC



data compression

Compressive sensing (CS)

- Shannon/Nyquist theorem is *pessimistic*
 - ▶ $2 \times$ bandwidth is the worst-case sampling rate — holds uniformly for *any* bandlimited data
 - ▶ sparsity/compressibility is irrelevant
 - ▶ Shannon sampling based on a linear model, compression based on a nonlinear model
- Compressive sensing
 - ▶ new sampling theory that *leverages compressibility*
 - ▶ key roles played by new *uncertainty principles* and *randomness*

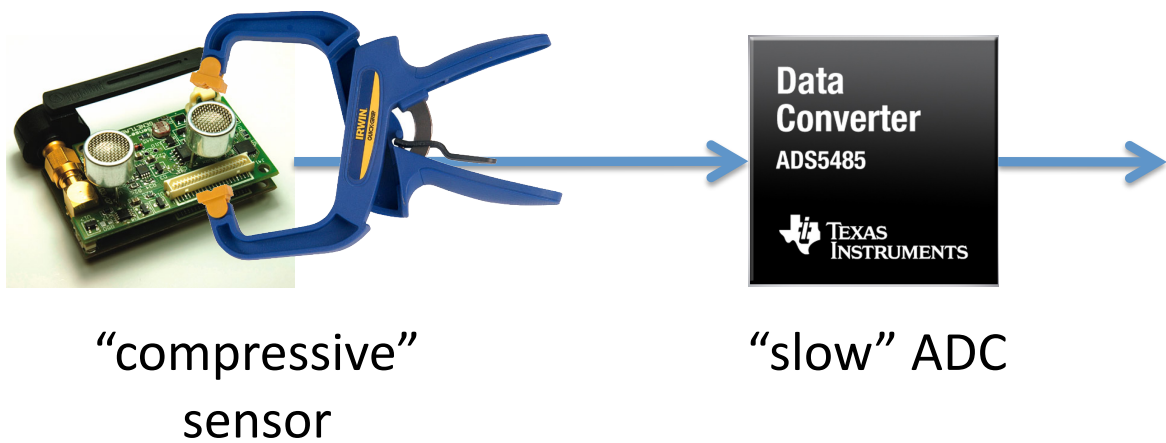


Shannon



Heisenberg

Compressive sensing



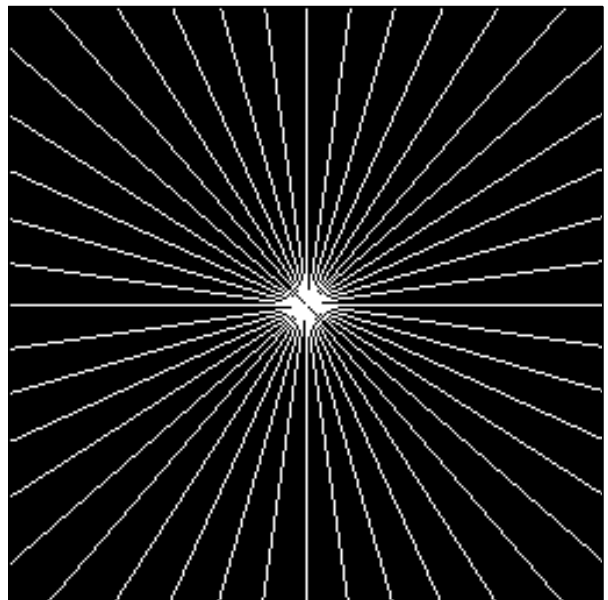
- Essential idea:
“pre-coding” the signal in analog makes it “easier” to acquire
- Reduce power consumption, hardware complexity, acquisition time

A simple underdetermined inverse problem

Observe a subset Ω of the 2D discrete Fourier plane



phantom (hidden)



white star = sample locations

$N := 512^2 = 262,144$ pixel image

observations on 22 radial lines, 10,486 samples, $\approx 4\%$ coverage

Minimum energy reconstruction

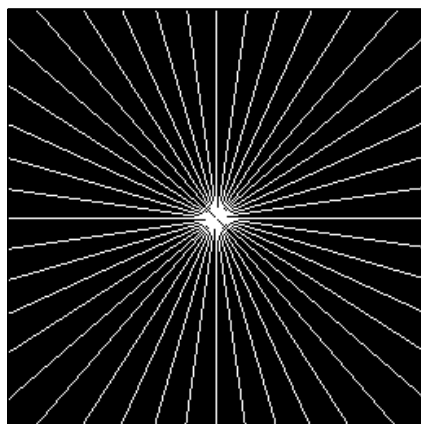
Reconstruct g^* with

$$\hat{g}^*(\omega_1, \omega_2) = \begin{cases} \hat{f}(\omega_1, \omega_2) & (\omega_1, \omega_2) \in \Omega \\ 0 & (\omega_1, \omega_2) \notin \Omega \end{cases}$$

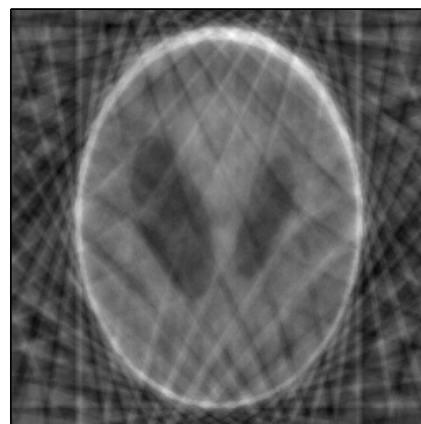
Set unknown Fourier coeffs to zero, and inverse transform



original



Fourier samples



g^*

Total-variation reconstruction

Find an image that

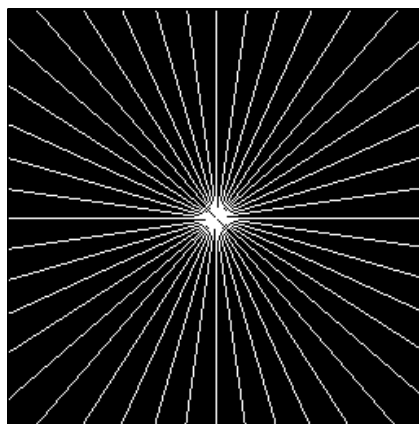
- Fourier domain: *matches observations*
- Spatial domain: has a *minimal amount of oscillation*

Reconstruct g^* by solving:

$$\min_g \sum_{i,j} |(\nabla g)_{i,j}| \quad \text{s.t.} \quad \hat{g}(\omega_1, \omega_2) = \hat{f}(\omega_1, \omega_2), \quad (\omega_1, \omega_2) \in \Omega$$



original



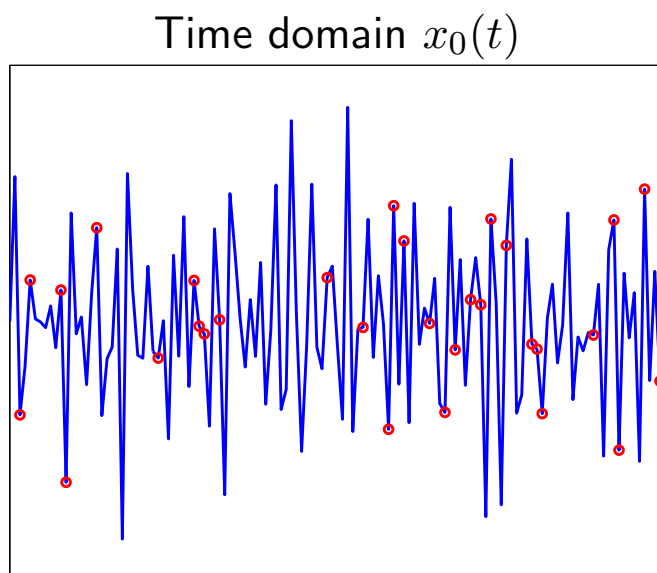
Fourier samples



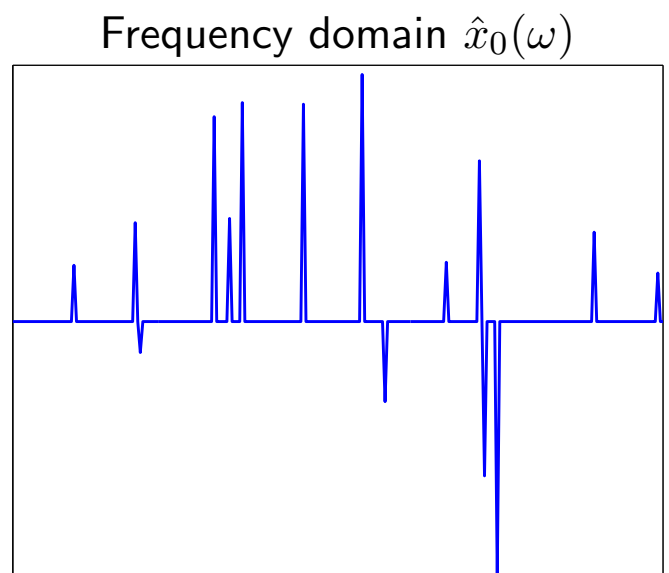
$g^* = \text{original}$
perfect reconstruction

Sampling a superposition of sinusoids

We take M samples of a superposition of S sinusoids:



Measure M samples
(red circles = samples)

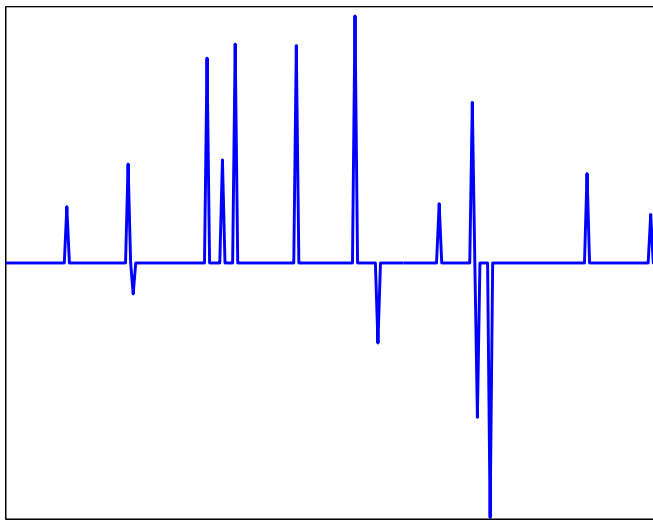


S nonzero components

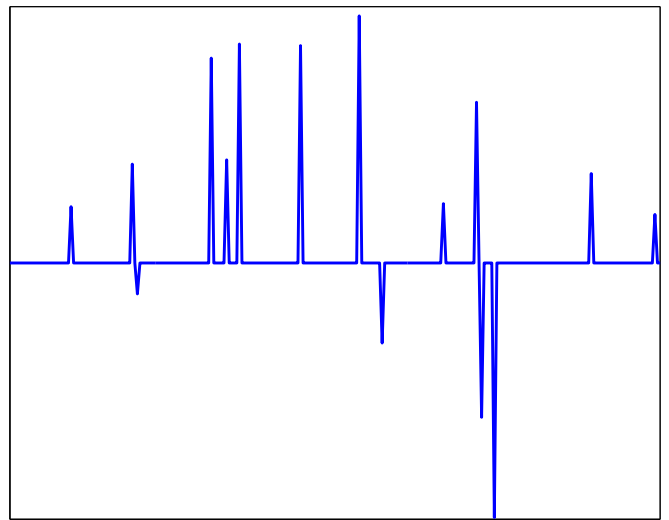
Sampling a superposition of sinusoids

Reconstruct by solving

$$\min_x \|\hat{x}\|_{\ell_1} \quad \text{subject to} \quad x(t_m) = x_0(t_m), \quad m = 1, \dots, M$$



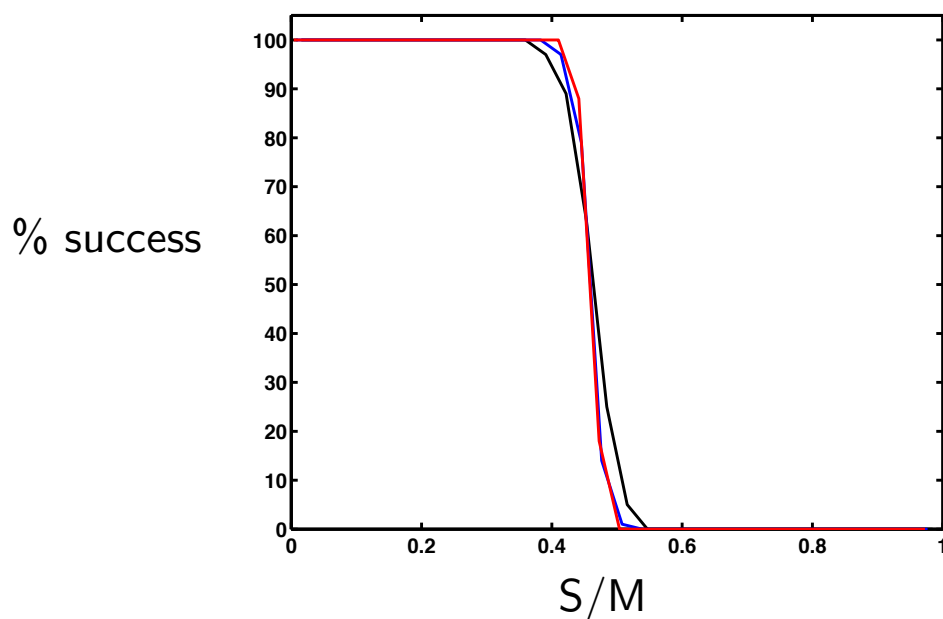
original \hat{x}_0 , $S = 15$



perfect recovery from 30 samples

Numerical recovery curves

- Resolutions $N = 256, 512, 1024$ (black, blue, red)
- Signal composed of S randomly selected sinusoids
- Sample at M randomly selected locations



- In practice, perfect recovery occurs when $M \approx 2S$ for $N \approx 1000$

A nonlinear sampling theorem

Exact Recovery Theorem (Candès, R, Tao, 2004):

- Unknown \hat{x}_0 is supported on set of size S
- Select M sample locations $\{t_m\}$ “at random” with

$$M \geq \text{Const} \cdot S \log N$$

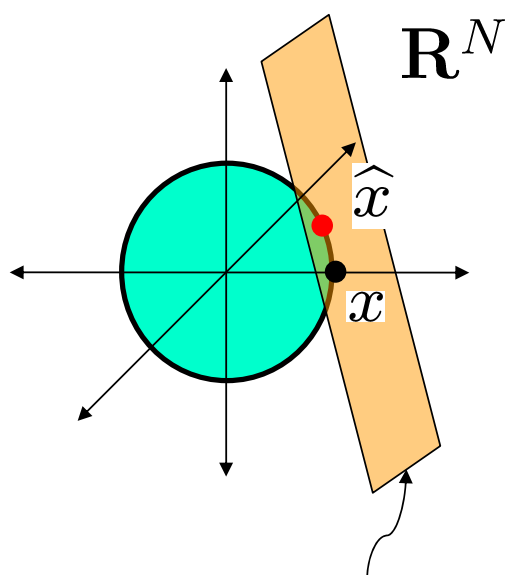
- Take time-domain samples (measurements) $y_m = x_0(t_m)$
- Solve

$$\min_x \|\hat{x}\|_{\ell_1} \quad \text{subject to} \quad x(t_m) = y_m, \quad m = 1, \dots, M$$

- Solution is **exactly** f with extremely high probability
- In total-variation/phantom example, S =number of jumps

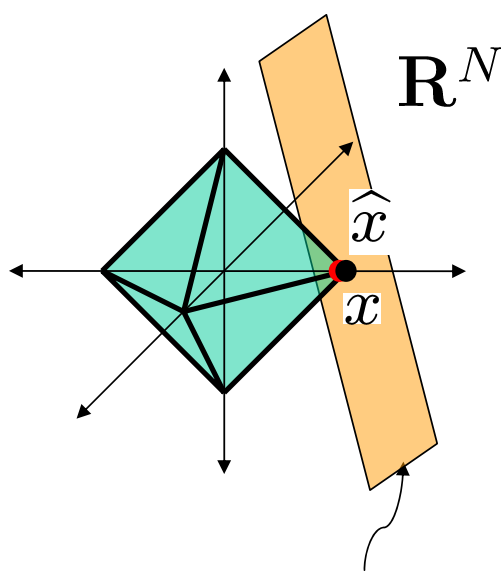
Graphical intuition for ℓ_1

$$\min_x \|x\|_2 \quad \text{s.t.} \quad \Phi x = y$$



$$\{x' : y = \Phi x'\}$$

$$\min_x \|x\|_1 \quad \text{s.t.} \quad \Phi x = y$$



$$\{x' : y = \Phi x'\}$$

Acquisition as linear algebra

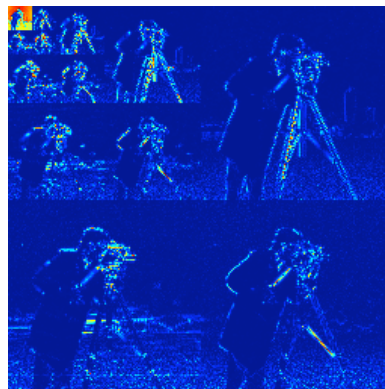
The diagram illustrates the linear algebra model for signal acquisition. It shows the equation $y = \Phi x$ with various annotations:

- y : A vertical vector labeled "data". To its left, a vertical blue line with dots at the ends is labeled "# samples" and M .
- Φ : A matrix labeled "acquisition system" below it.
- x : A vertical vector labeled "unknown signal/image" below it. To its right, a vertical blue line with dots at the ends is labeled "resolution/ bandwidth" and N .

- Small number of samples = underdetermined system
Impossible to solve in general
- If x is *sparse* and Φ is *diverse*, then these systems can be “inverted”

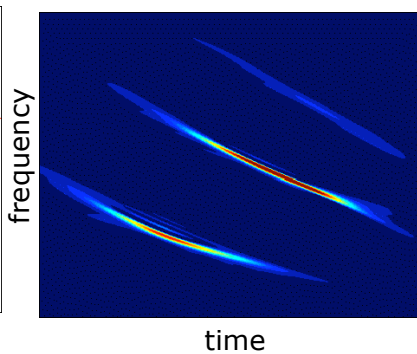
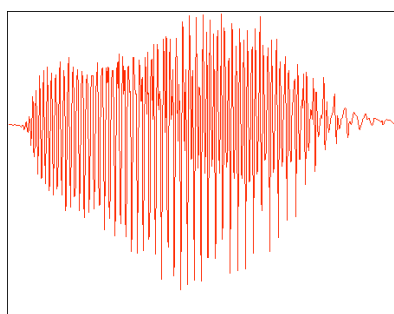
Sparsity/Compressibility

N
pixels



$S \ll N$
large
wavelet
coefficients

N
wideband
signal
samples



$S \ll N$
large
Gabor
coefficients

Wavelet approximation

Take 1% of *largest* coefficients, set the rest to zero (adaptive)

original



approximated



rel. error = 0.031

Linear measurements

- Instead of samples, take *linear measurements* of signal/image x_0

$$y_1 = \langle x_0, \phi_1 \rangle, \quad y_2 = \langle x_0, \phi_2 \rangle, \quad \dots, y_M = \langle x_0, \phi_K \rangle$$

$$y = \Phi x_0$$

- Equivalent to transform-domain sampling,
 $\{\phi_m\}$ = basis functions
- Example: **pixels**



Linear measurements

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$$y = \Phi x_0$$

- Equivalent to transform-domain sampling,
 $\{\phi_m\}$ = basis functions
- Example: **line integrals** (tomography)

$$y_m = \left\langle \text{CT scan image}, \text{line integral mask} \right\rangle$$


Linear measurements

- Instead of samples, take *linear measurements* of signal/image x_0

$$y_1 = \langle x_0, \phi_1 \rangle, \quad y_2 = \langle x_0, \phi_2 \rangle, \quad \dots, y_M = \langle x_0, \phi_K \rangle$$

$$y = \Phi x_0$$

- Equivalent to transform-domain sampling,
 $\{\phi_m\}$ = basis functions
- Example: **sinusoids** (MRI)

$$y_m = \left\langle \text{MRI Image}, \text{Sinusoid} \right\rangle$$