

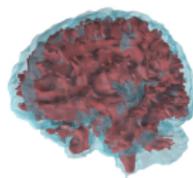
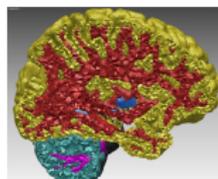
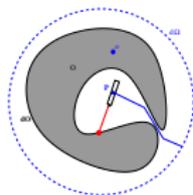
Sampling and Meshing Curved 3D Domains by Delaunay Refinement

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ENS-Lyon
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Applications

- ▶ visualization and graphics applications
- ▶ CAD and reverse engineering
- ▶ geometric modelling in medicine, geology, biology etc.
- ▶ autonomous exploration and mapping (SLAM)
- ▶ scientific computing : meshes for FEM



Two main issues

Sampling

- ▶ How do we choose points in the domain ?
- ▶ What information do we need to know/measure about the domain ?

Topology and Geometry

1. How do we connect the points ?
2. Under what sampling conditions can we compute a good approximation of the domain ?
3. What is a good approximation ?

State of the art : implicit surface meshing

Marching cube

Lorensen & Cline [87]

Lopez & Brodlie [03] : topological consistency

Plantiga & Vegter [04] : certified topology using interval arithmetic

Morse theory

Stander & Hart [97]

B., Cohen-Steiner & Vegter [04] : certified topology

Delaunay refinement

Ruppert [95]

Shewchuk [02]

Chew [93]

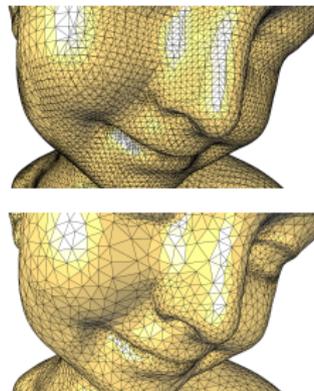
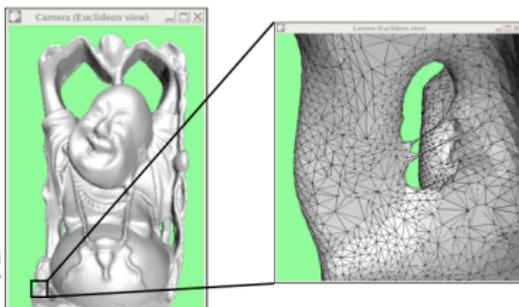
B. & Oudot [03,04]

Cheng et al. [04]

Overview

- ▶ What is a good approximation of a surface ?
- ▶ Restricted Delaunay triangulation
- ▶ Surface mesh generation
- ▶ Extensions and applications

What is a good approximation of a surface ?



Topological equivalence

Homeomorphism

Two subsets X and Y of \mathbb{R}^d are said to be **homeomorphic** if there exists a continuous, bijective map $f : X \rightarrow Y$ with continuous inverse f^{-1} .

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Isotopy

Two subsets X and Y of \mathbb{R}^d are said to be **isotopic** if there exists a continuous map $f : X \times [0, 1] \rightarrow \mathbb{R}^d$ such that $f(\cdot, 0)$ is the identity of X , $f(X, 1) = Y$, and for each $t \in [0, 1]$, $f(\cdot, t)$ is a homeomorphism onto its image.

Distance between two sets

Hausdorff distance

$$d_H(X, Y) = \max(\sup_{x \in X} d(x, Y), \sup_{y \in Y} d(y, X))$$

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$$d_{\mathcal{F}}(X, Y) = \inf_h \sup_{p \in X} d(p, h(p))$$

where h ranges over all homeomorphisms from X to Y

Distance between two sets

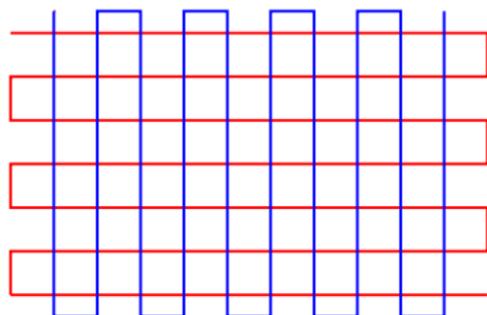
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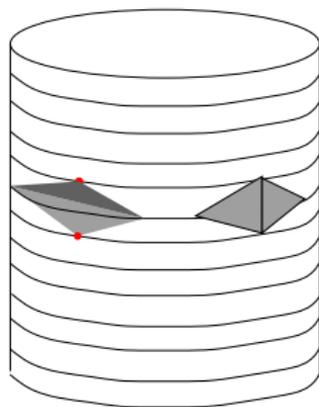
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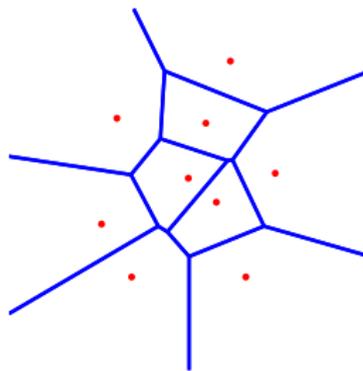
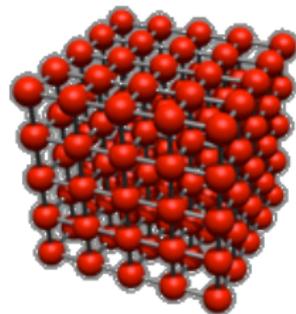
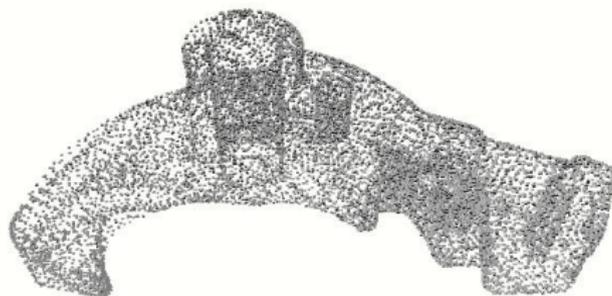
Other guarantees

- ▶ Approximation of normals
- ▶ Approximation of areas
- ▶ Approximation of curvatures
- ▶ Aspect ratio of the facets



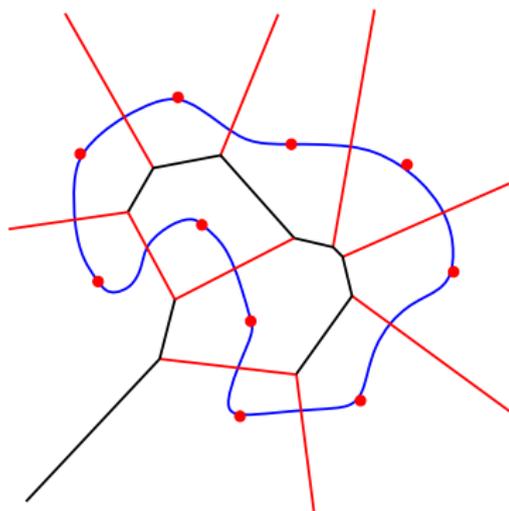
Restricted Delaunay triangulation

Data structuring by space subdivision



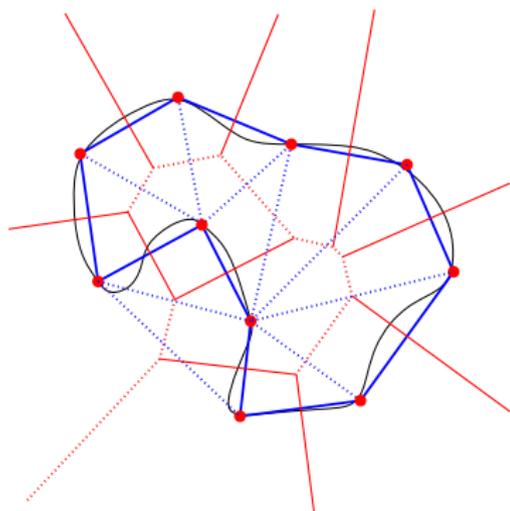
Definition

The **restricted Delaunay triangulation** $\text{Del}_{|\mathcal{S}}(\mathcal{P})$ is the set of simplices of the Delaunay triangulation whose dual Voronoi faces intersect \mathcal{S}



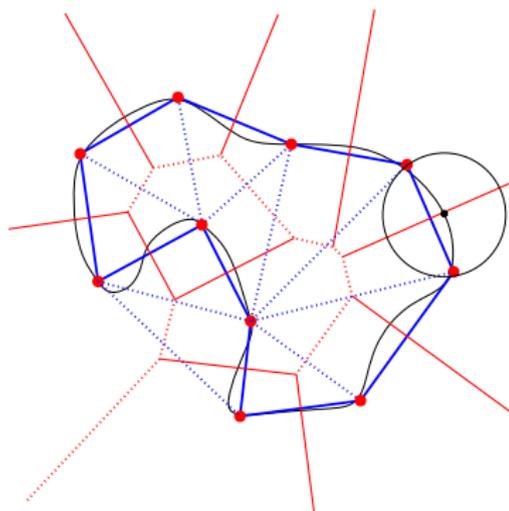
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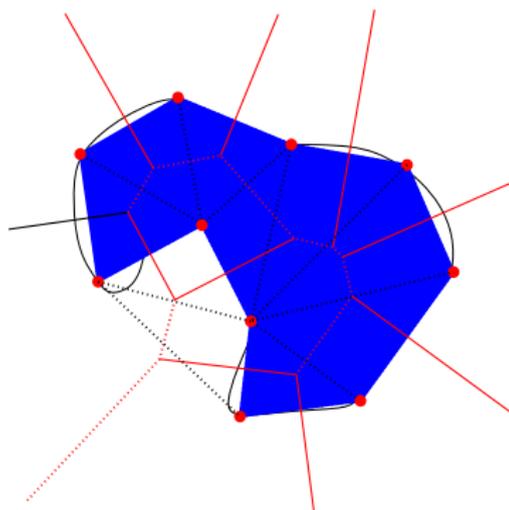
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Definition

The **restricted Delaunay triangulation** $\text{Del}_{|O}(\mathcal{P})$ is the set of simplices of the Delaunay triangulation whose dual Voronoi faces belong to $\text{Vor}_{|O}(\mathcal{P})$



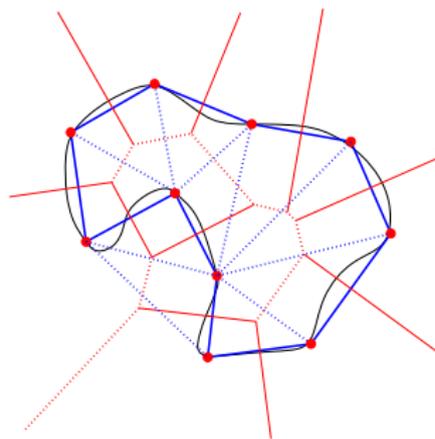
A variant of the nerve theorem

Theorem [Edelsbrunner & Shah 1997]

If S is compact and without boundary and if, for any face $f \in \text{Vor}_I S(E)$,

1. f intersects S transversally
2. $f \cap S = \emptyset$ or is a topological ball

then $\text{Del}_I S(E) \approx S$



Homeomorphism

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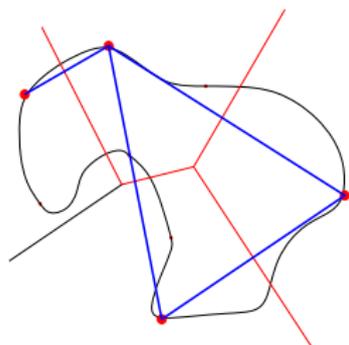
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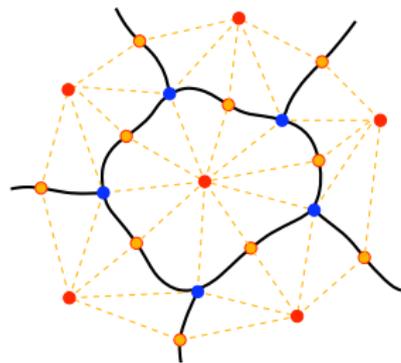
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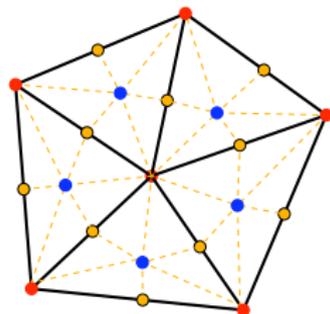
Proof of the closed ball property

Barycentric subdivision

of $\text{Vor}_S(E)$

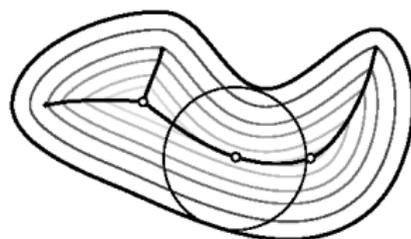


of $\text{Del}_S(E)$



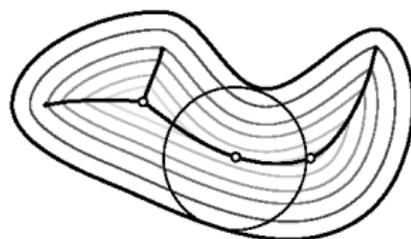
Local feature size

- ▶ Medial axis of \mathcal{S} : $M(\mathcal{S})$
set of points with at least two closest points on \mathcal{S}
- ▶ Local feature size : $\text{Ifs}(x)$
 $\forall x \in \mathcal{S}, \text{Ifs}(x) = d(x, M(\mathcal{S}))$



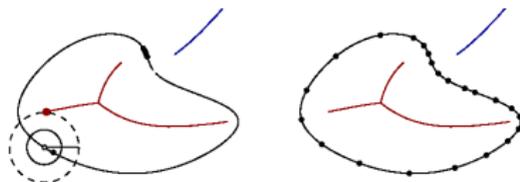
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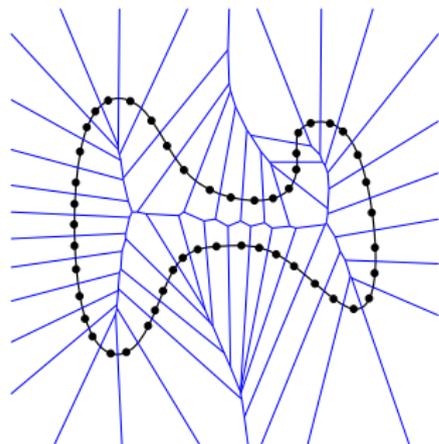
ϵ -sample of \mathcal{S} (ϵ -covering)

$$\mathcal{P} \subset \mathcal{S}, \forall x \in \mathcal{S} = d(x, \mathcal{P}) \leq \epsilon \text{Ifs}(x)$$



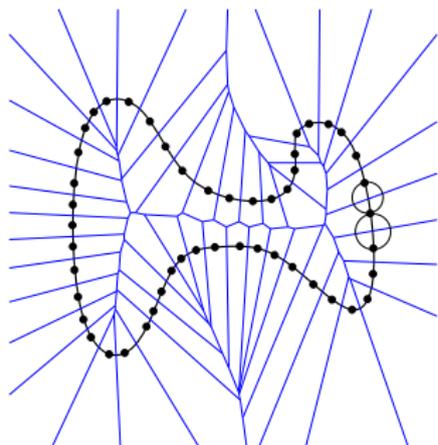
Restricted Delaunay triangulations of ε -samples

[Amenta et al. 1998-]



If \mathcal{P} is an ε -sample of a $C^{1,1}$ surface
 $\mathcal{S} \subset \mathbb{R}^3$, $\varepsilon \leq 0.12$

- ▶ $\text{Del}_{|\mathcal{S}}(\mathcal{P})$ provides good estimates of
 - ▶ normals
 - ▶ areas
 - ▶ curvature [Cohen-Steiner, Morvan]
- ▶ There exists an isotopy
 $\phi : \text{Del}_{|\mathcal{S}}(\mathcal{P}) \rightarrow \mathcal{S}$
- ▶ $\sup_x (\|\phi(x) - x\|) = O(\varepsilon^2)$

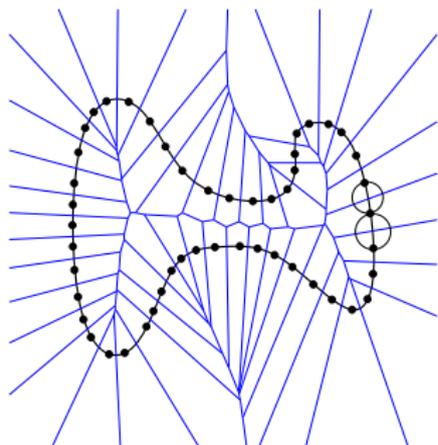


Definition

1. $\text{Del}_{|S}(\mathcal{P})$ has a vertex on each connected component of S
2. for any circumscribing ball $B_f = (c_f, r_f)$ of any facet f of $\text{Del}_{|S}(\mathcal{P})$, $r_f \leq \varepsilon \text{ lfs}(c_f)$

Loose ε -samples

[B. & Oudot 2005]



Definition

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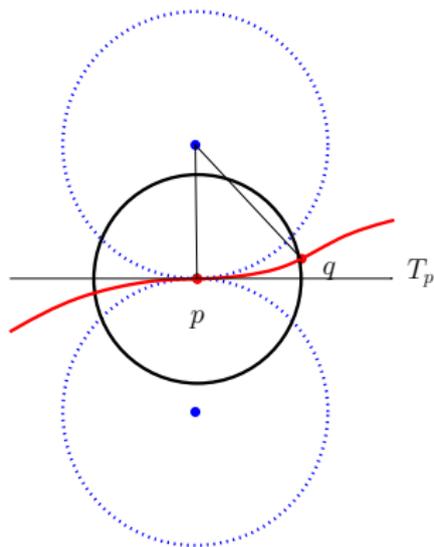
Loose ε -samples are $\varepsilon(1 + O(\varepsilon^2))$ -samples

Sketch of proofs

Surfaces : local properties 1/2

Chord lemma

$$\forall p, q \in \mathcal{S}, \|p - q\| \leq 2\epsilon \text{fs}(p) \Rightarrow \sin(\angle pq, T_p) \leq \epsilon$$

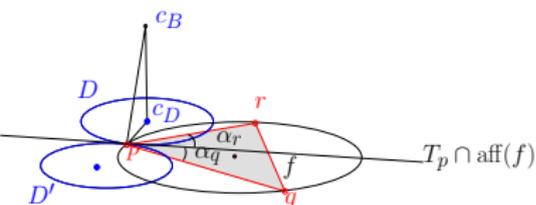


Surfaces : local properties 2/2

Facet normal lemma

Let $f = pqr$ be a facet of $\text{Del}(\mathcal{P})$ and assume that $\hat{p} \geq \frac{\pi}{3}$. If the circumradius ρ_f of f is at most $\varepsilon \text{lfs}(p)$, then $\sin(n_f, n_p) \leq 2\varepsilon$.

Proof



$$\sin(n_f, n_p) = \sin(\angle pc_B c_D) = \frac{\|p - c_D\|}{\|p - c_B\|} = \frac{\rho_D}{\text{lfs}(p)}$$

$$\hat{p} = \alpha_q + \alpha_r \geq \frac{\pi}{3} \stackrel{\text{wlog}}{\Rightarrow} \alpha_q \geq \frac{\pi}{6}$$

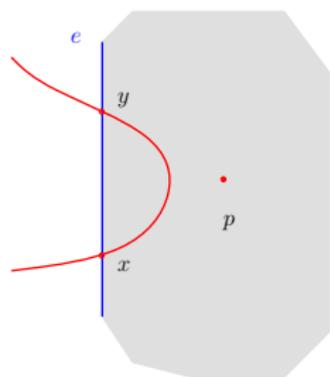
$$q \notin D \cup D' \Rightarrow \|p - q\| \geq 2\rho_D \sin \alpha_q \geq \rho_D$$

$$\frac{\rho_D}{\text{lfs}(p)} \leq \frac{\|p - q\|}{\text{lfs}(p)} \leq \frac{2\rho_f}{\text{lfs}(p)} \leq 2\varepsilon$$

Proof of homeomorphism (sketch)

The conditions of the Nerve Th. are satisfied

1. Any edge of $\text{Vor}_S(\mathcal{P})$ intersects S in one point



$$\begin{aligned} \|x - p\| &\leq \varepsilon \text{Ifs}(x) \\ \|y - p\| &\leq \varepsilon \text{Ifs}(y) \leq \frac{\varepsilon}{1-\varepsilon} \text{Ifs}(x) \\ \Rightarrow \|x - y\| &\leq 2 \frac{\varepsilon}{1-\varepsilon} \text{Ifs}(x) \\ \Rightarrow [xy] &\perp n_x \approx n_p \end{aligned} \quad (*)$$

$$\begin{aligned} [xy] &\perp e^* \text{ and the facet lemma} \\ \Rightarrow [xy] &\parallel n_p \end{aligned}$$

2. Similar arguments show that faces of higher dimensions are also topological balls

$\pi : \text{Del}_{|\mathcal{S}}(\mathcal{P}) \rightarrow \mathcal{S}$ is injective

$x \in \mathcal{S}$

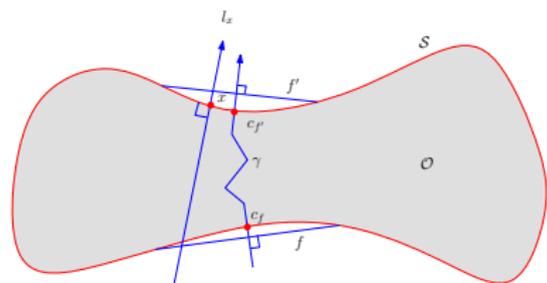
n_x the normal to \mathcal{S} at x

I_x the normal fiber $[x - r n_x, x + r n_x]$ where $r = \varepsilon \text{ lfs}(x)$

Injectivity lemma

If \mathcal{P} is a loose ε -sample for $\varepsilon \leq 0.12$, then I_x intersects $\text{Del}_{|\mathcal{S}}$ in at most one point

Proof of the injectivity lemma (by contradiction)



f, f' two consecutive facets of $\text{Del}_{|S}(\mathcal{P})$ that intersect l_x

$T = t_1, \dots, t_s$ the set of tet. intersected by l_x between f and f'

$\gamma = (c_f = c_0, c_1, \dots, c_s, c_{f'} = c_{s+1})$
 $c_i = \text{cc of } t_i, \gamma \subset \text{skel}(\text{Vor}(\mathcal{P}))$

with $s_i = (c_{i+1} - c_i) / \|c_{i+1} - c_i\|$

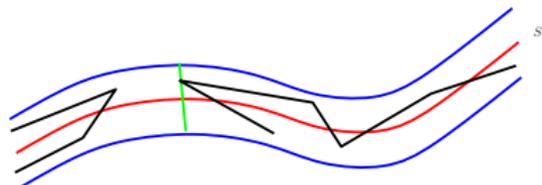
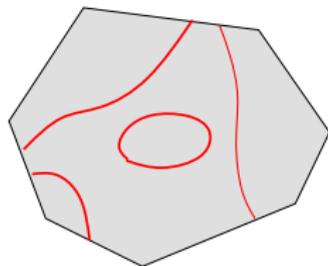
- ▶ c_f and $c_{f'}$ are consecutive points of $l_x \cap S$
 $\Rightarrow (n_{c_f} \cdot s_f) \times (n_{c_{f'}} \cdot s_{f'}) < 0$
- ▶ Facet normal lemma
 $\Rightarrow (n_{c_f} \cdot s_f) \times (n_{c_{f'}} \cdot s_{f'}) < -1 + O(\varepsilon^2)$
- ▶ Delaunay $\Rightarrow (n_x \cdot s_i) \times (n_x \cdot s_{i+1}) > 0$
 $\Rightarrow (n_x \cdot s_f) \times (n_x \cdot s_{f'}) > 0$
- ▶ Normal variation lemma
 $\Rightarrow n_{c_f} \approx n_x \approx n_{c_{f'}}$
- ▶ Contradiction !

$\pi : \text{Del}_S(\mathcal{P}) \rightarrow \mathcal{S}$ is surjective

If \mathcal{P} is a loose ε -sample of \mathcal{S} with $\varepsilon \leq 1.12$, then \mathcal{S} is covered at least once by π

Proof

- ▶ any edge of $\text{Del}_S(\mathcal{P})$ belongs to exactly two facets of $\text{Del}_S(\mathcal{P})$
- ▶ every cc of \mathcal{S} contains ≥ 1 vertex of $\text{Del}_S(\mathcal{P})$
- ▶ by contradiction : there exists an edge where the injectivity lemma is violated



Isotopy

If \mathcal{P} is an ε -sample for $\varepsilon \leq 0.12$, π induces an isotopy that maps $\text{Del}_{|\mathcal{S}}(\mathcal{P})$ to \mathcal{S}

The isotopy moves the points by $O(\varepsilon^2)$

Isotopy

If \mathcal{P} is an ε -sample for $\varepsilon \leq 0.12$, π induces an isotopy that maps $\text{Del}_{|\mathcal{S}}(\mathcal{P})$ to \mathcal{S}

The isotopy moves the points by $O(\varepsilon^2)$

Proof

- ▶ **Homeomorphism:** π is bijective and bicontinuous
- ▶ **Isotopy :** $f : \text{Del}_{|\mathcal{S}}(\mathcal{P}) \times [0, 1] \rightarrow \mathcal{S}, f(x, t) = x + t \frac{\pi(x) - x}{\|\pi(x) - x\|}$
- ▶ **Fréchet distance :** trivially $\leq \varepsilon \sup_{x \in \mathcal{S}} \text{Ifs}(x)$
for a better bound, adapt the chord lem.

Surface mesh generation by Delaunay refinement

Surface mesh generation by Delaunay refinement

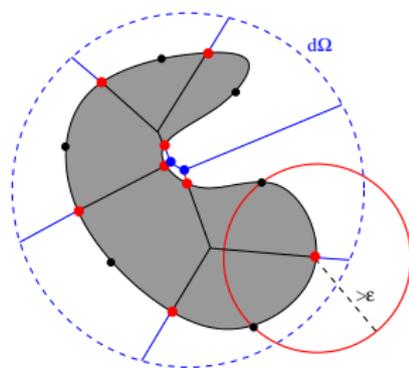
$\phi : \mathcal{S} \rightarrow \mathbb{R} = \text{Lipschitz function}$

$$\forall x \in \mathcal{S}, 0 < \phi_{\min} \leq \phi(x) < \epsilon \text{ lfs}(x)$$

ORACLE : For a facet f of $\text{Del}_{|\mathcal{S}}(\mathcal{P})$,
return c_f , r_f and $\phi(c_f)$

A facet f is **bad** if $r_f > \phi(c_f)$

[Chew 1993, B. & Oudot 2003]



Surface mesh generation by Delaunay refinement

$\phi : S \rightarrow \mathbb{R} =$ Lipschitz function
 $\forall x \in S, 0 < \phi_{\min} \leq \phi(x) < \epsilon \text{ifs}(x)$

[Chew 1993, B. & Oudot 2003]

ORACLE : For a facet f of $\text{Del}_1 S(\mathcal{P})$,
return c_f, r_f and $\phi(c_f)$

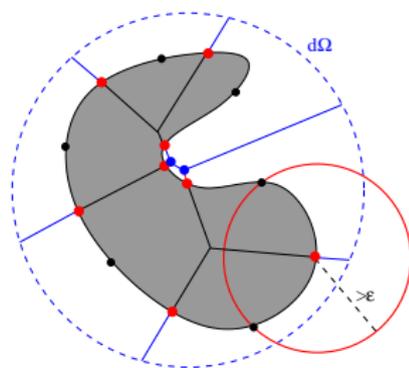
A facet f is **bad** if $r_f > \phi(c_f)$

Algorithm

INIT compute an initial (small) sample $\mathcal{P}_0 \subset S$

REPEAT IF f is a bad facet
 insert_in_Del3D(c_f)
 update \mathcal{P} and $\text{Del}_1 S(\mathcal{P})$

UNTIL all facets are good



The algorithm terminates

Properties of the output

- ▶ The output sample \mathcal{P} is
 - ▶ a covering : (loose ε -sample)
 $\forall x \in \mathcal{S}, d(x, \mathcal{P}) \leq \phi(x)(1 + O(\phi^2(x))) \leq \varepsilon(1 + O(\varepsilon^2) \text{Ifs}(x))$
 - ▶ a packing : $\forall p \in \mathcal{P}, d(p, \mathcal{P} \setminus \{p\}) \geq \min(\phi(p), \phi(q))$
 $\geq \phi(p) - \|p - q\|$
 $\geq \frac{1}{2} \phi(p)$
- ▶ $|\mathcal{P}| = O\left(\int_{\mathcal{S}} \frac{dx}{\phi^2(x)}\right)$
- ▶ $\text{Del}_{|\mathcal{S}}(\mathcal{P})$ is a good approximation of \mathcal{S}
- ▶ all facets have a bounded aspect ratio $\frac{r_f}{l_f} \leq \frac{\phi(c_f)}{\min_{x \in \text{vert}(f)} \phi(x)}$

$$\text{Size of the sample} = O\left(\int_S \frac{dx}{\phi^2(x)}\right)$$

Proof

Let $\rho(x) = \inf\{r : |B(x, r) \cap \mathcal{P}| = 2\}$ and $B_p = B(p, \frac{\rho(p)}{2})$, $p \in \mathcal{P}$

$$\begin{aligned} \int_S \frac{dx}{\rho^2(x)} &\geq \sum_p \int_{(B_p \cap S)} \frac{dx}{\rho^2(x)} && \text{(the } B_p \text{ are disjoint)} \\ &\geq \frac{4}{9} \sum_p \frac{\text{area}(B_p \cap S)}{\rho^2(p)} && \rho(x) \leq \rho(p) + \|p - x\| \\ &\geq \frac{4}{9} \sum_p \frac{3}{16} \pi = \frac{\pi}{12} |\mathcal{P}| && \leq \frac{3}{2} \rho(p) \end{aligned}$$

$$\begin{aligned} \forall x \in B_p, \quad &\rho(x) \geq \rho(p) - \|x - p\| \geq \frac{1}{2} \rho(p) \\ &\rho(p) = \|p - q\| \geq \phi(p) - \|p - q\| \Rightarrow \rho(p) \geq \frac{\phi(p)}{2} \\ &\phi(x) \leq \phi(p) + \frac{\rho(p)}{2} \leq \frac{5}{2} \rho(p) \leq 5\rho(x) \end{aligned}$$

Less demanding oracle

$\text{Vor}_{|S}^{\pm}(\mathcal{P})$ = edges of $\text{Vor}(\mathcal{P})$ that intersect S
an **odd** number of times

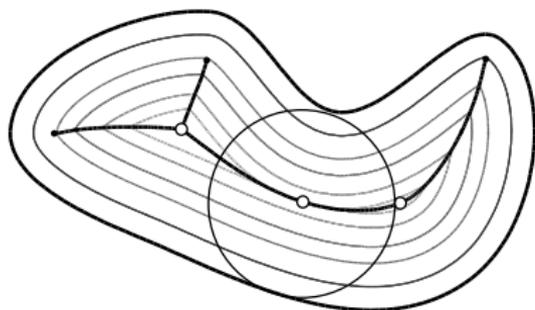
if $S = f^{-1}(x)$, deciding whether an edge $e = [pq]$ belongs to $\text{Vor}_{|S}^{\pm}(\mathcal{P})$ reduces to evaluating the sign of f at p and q

The isotopy proof still holds

Computing $\text{lfs}(x)$ is difficult

Computing $\text{rch}(S) = \inf_{x \in S} \text{lfs}(x)$ is much easier
 $\text{rch}(S)$ is either

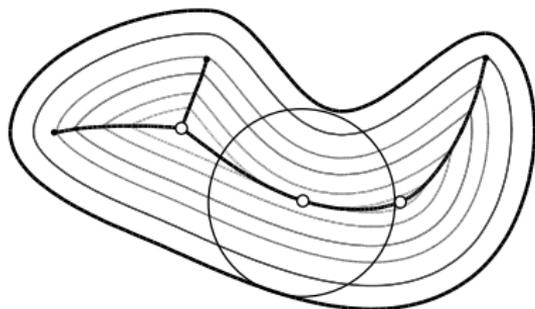
- ▶ a local minimum of the smallest radius of curvature or
- ▶ the radius of a sphere with a diameter binormal to S



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Computing $\text{rch}(S) = \inf_{x \in S} \text{lfs}(x)$ is much easier
 $\text{rch}(S)$ is either

- ▶ a local minimum of the smallest radius of curvature or
- ▶ the radius of a sphere with a diameter binormal to S



$$F(p) = 0$$

$$F(q) = 0$$

$$(p - q) \times \nabla f(p) = 0$$

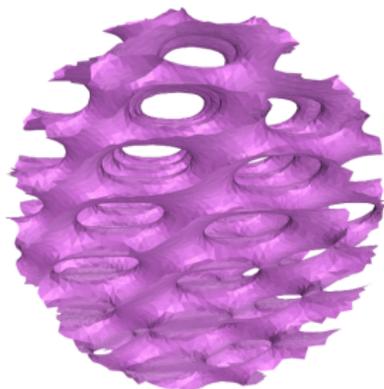
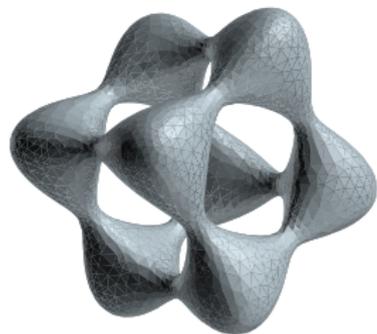
$$(p - q) \times \nabla f(q) = 0$$

$$\lambda (p - q)^2 = 1$$

Applications

- ▶ Implicit surfaces $f(x, y, z) = 0$
- ▶ Isosurfaces in a 3d image (Medical images)
- ▶ Triangulated surfaces (Remeshing)
- ▶ Point sets (Surface reconstruction)

Results on smooth implicit surfaces

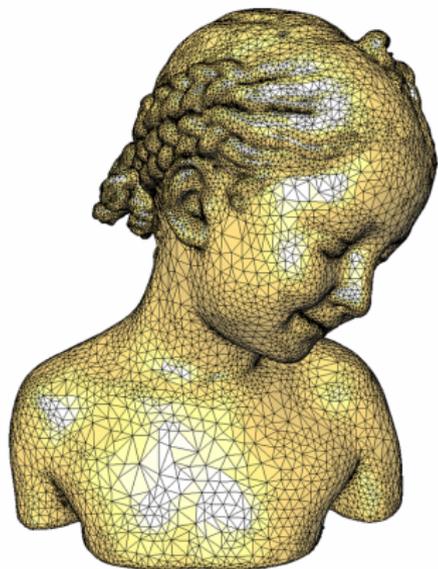


Pentium IV, 3.6GHz

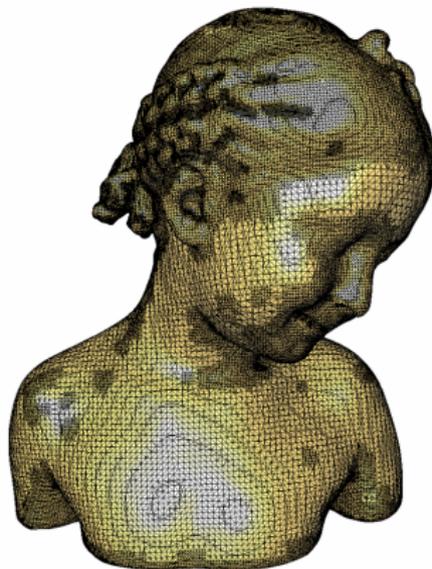
Surface	Output size	Combinatorial	Bipolar oracle	time	CPU time
Tangle cube	4,242	8.31%	0.81%	8.52%	2.42 s
Trefoil	8,317	12.54%	0.93%	13.47%	5.14 s

% are wrt $\text{Del}(\mathcal{P})$

Comparison with the Marching Cube algorithm

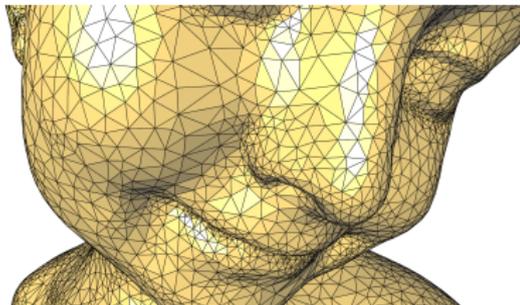


Delaunay Refinement

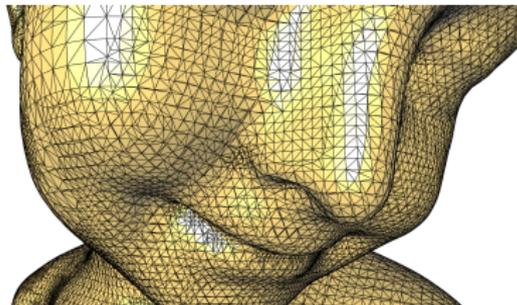


Marching Cube

Comparison with the Marching Cube algorithm

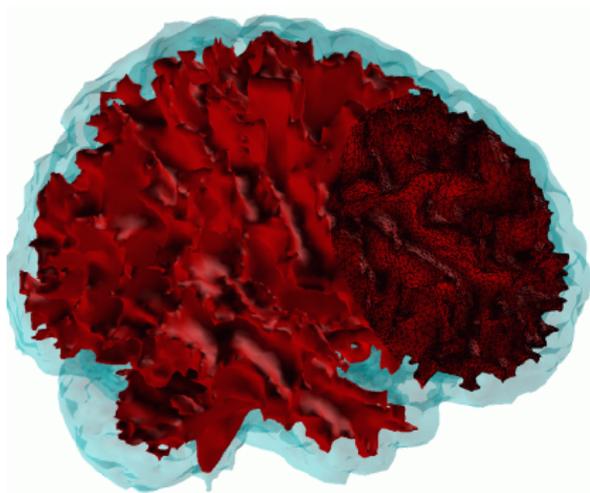
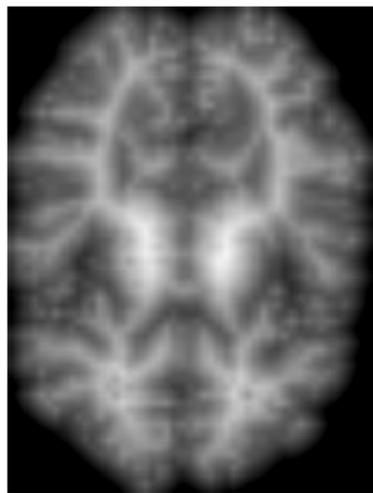


Delaunay refinement



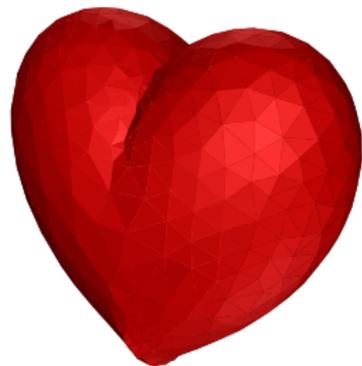
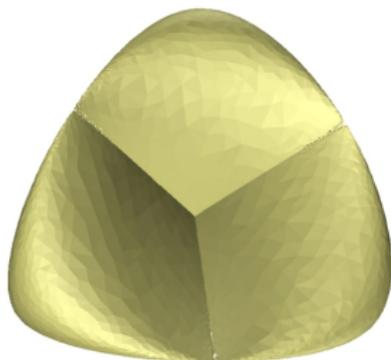
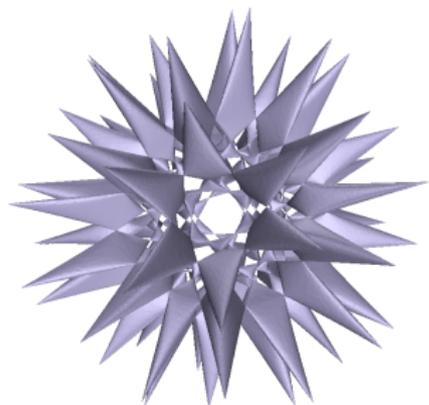
Marching cube

Contouring isosurfaces in 3D images



Collaboration with Asclepios, Caïman and Odyssee INRIA project-teams

Non smooth surfaces



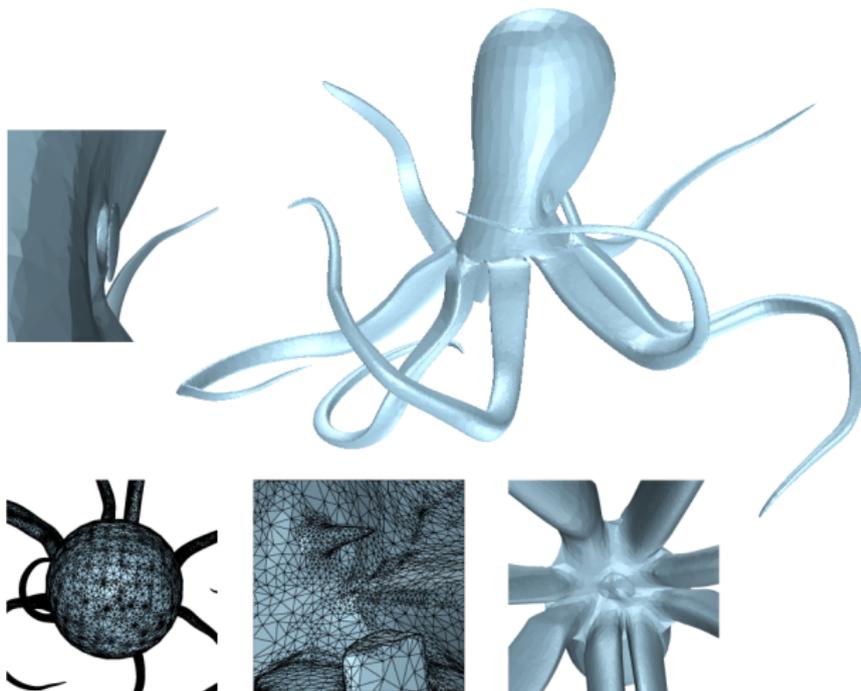
Extensions to

k -Lipschitz surfaces
piecewise smooth surfaces

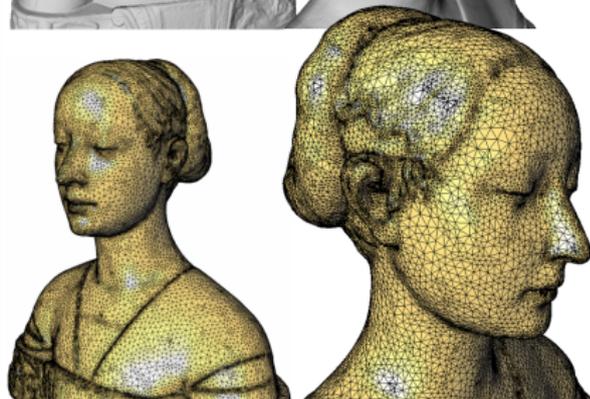
[B. Oudot 06]

[Dey et al., Rineau & Yvinec 07]

Remeshing Polyhedral Surfaces



Point set surfaces



Courtesy of P. Alliez

Extension to non-binary datasets

□ Partition of space $\mathcal{P} = \{\Omega_0, \Omega_1, \dots, \Omega_n\}$

$$\mathbb{R}^3 = \sqcup_{i \in \{0, \dots, n\}} \Omega_i$$

□ Boundaries $\Gamma = \cup_i \delta\Omega_i$

□ E a “good” point sample of Γ

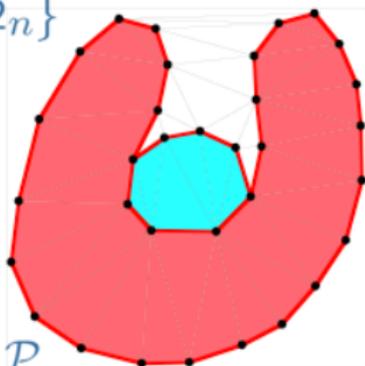
□ Partition of Delaunay tetrahedra induced by \mathcal{P}

$$\text{Del}|_{\mathcal{P}}(E) = \{\text{Del}|_{\Omega_0}(E), \dots, \text{Del}|_{\Omega_n}(E)\}$$

= each tetrahedron is labeled with the tissue its circumcenter belongs to

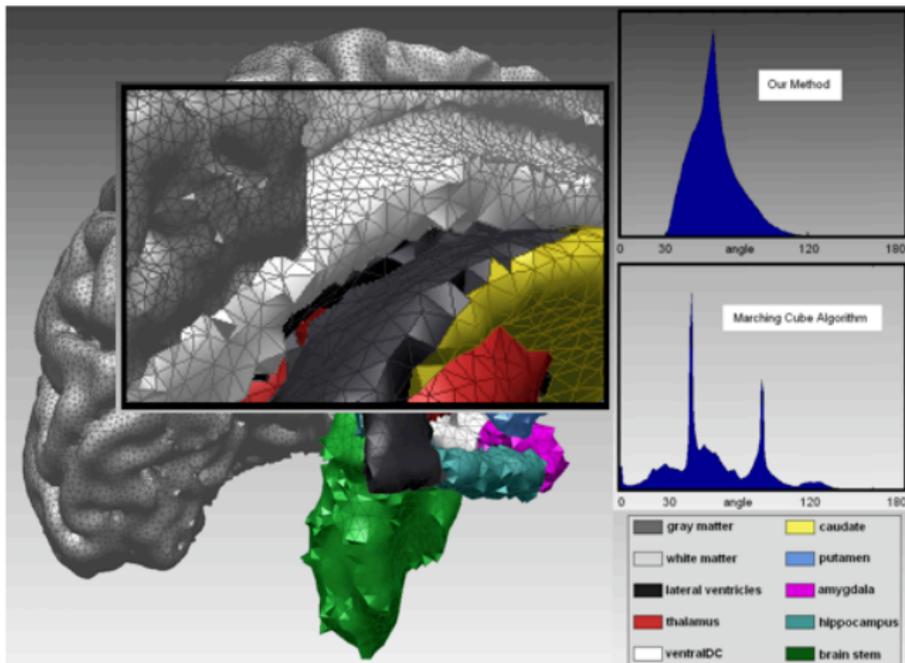
➔ **Consistent triangular and tetrahedral meshes**

□ It “suffices” to generate E !



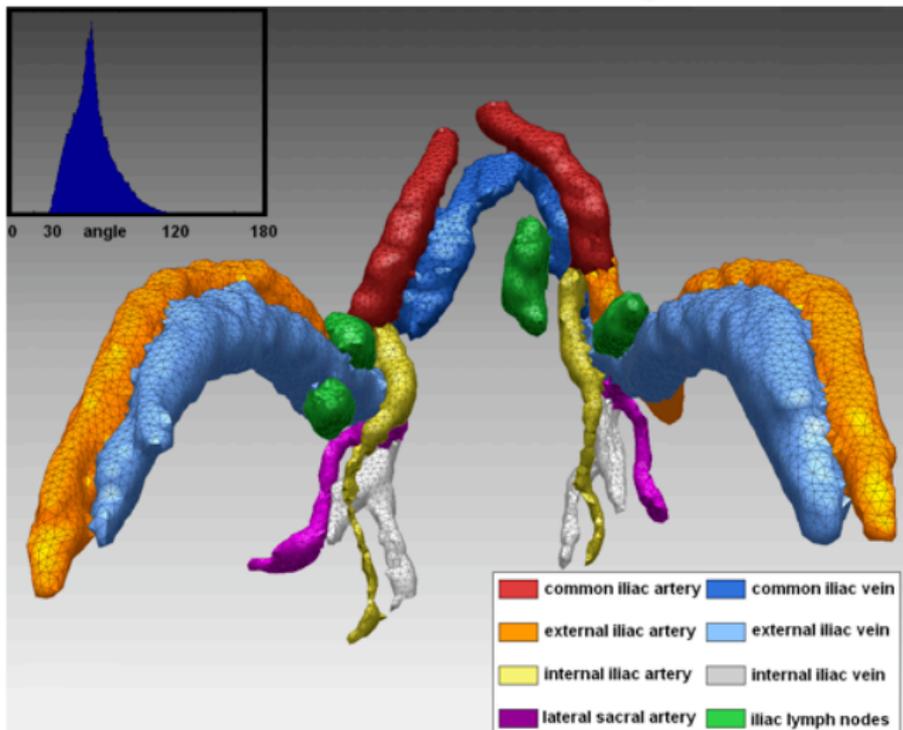
Results: Surface meshing with tissue-dependent resolution

- 72 tissues
- 112K vertices
- 228K b. facets
- 728K tets
- 340 seconds
- Criteria:
 - min angle $>30^\circ$
 - cortex size $<1\text{mm}$
 - others size $<2\text{mm}$

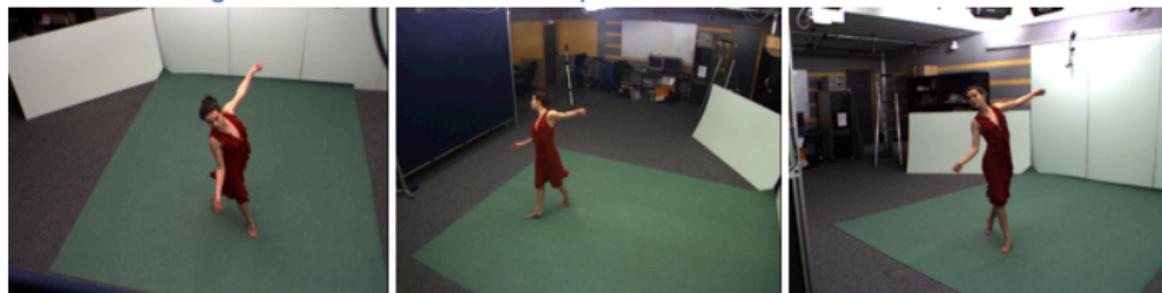


Results: Uniform surface meshing

- 15 tissues
- 11K vertices
- 23K b. facets
- 73K tets
- 35 seconds
- Criteria:
 - min angle $>30^\circ$
 - size $<1\text{mm}$



- **Multi-view 3D reconstruction:** Recovering the **3D shape** of an object from **several images** taken from **different viewpoints**



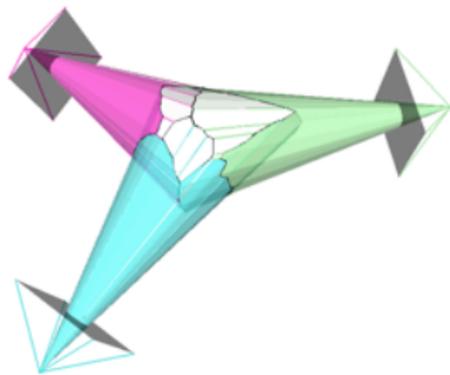
- **Shape-from-silhouettes:** Only uses **foreground/background** segmentations



Problem statement

- **Visual hull:** Intersection of the visual cones of the different cameras

- 😊 Very fast
- ☹️ Coarse reconstruction: OK for rendering



- Previous work

- ↳ *Volumetric methods*

- 😊 Fast, straightforward
- ☹️ High memory cost
- ☹️ Huge output mesh
- ☹️ Discretization artefacts (stair-casing effect)

- ↳ *Exact polyhedral intersection* (Franco & Boyer, 2003)

- 😊 Very fast
- ☹️ Low quality mesh
- ☹️ Noisy/inconsistent silhouettes ➔ numerical instabilities

Delaunay meshing approach

□ Multi-view oracle:

A Delaunay tetrahedron is part of the approx. visual hull



Its circumcenter projects inside the silhouette in all views

□ Refinement criterion = reprojection error

A boundary facet is good



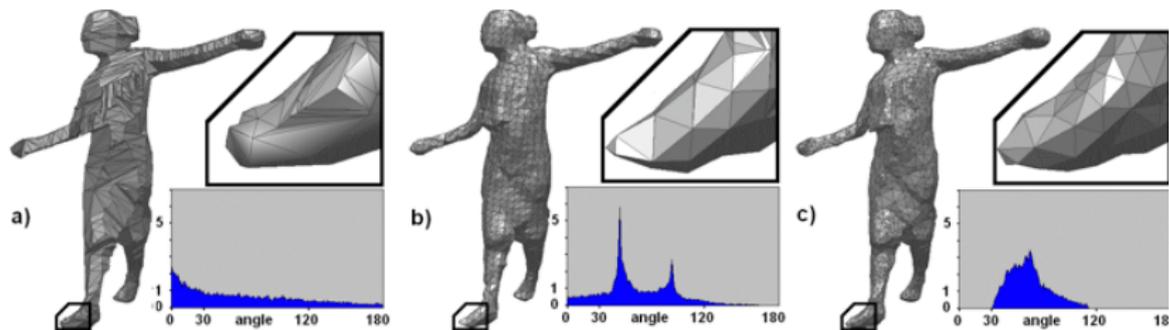
All projections are closer from the silhouette boundary than a user-defined threshold in all views

□ Pros and cons

☹ Slower

😊 High quality mesh

😊 Reprojection error control (one-sided)



Polyhedral intersection

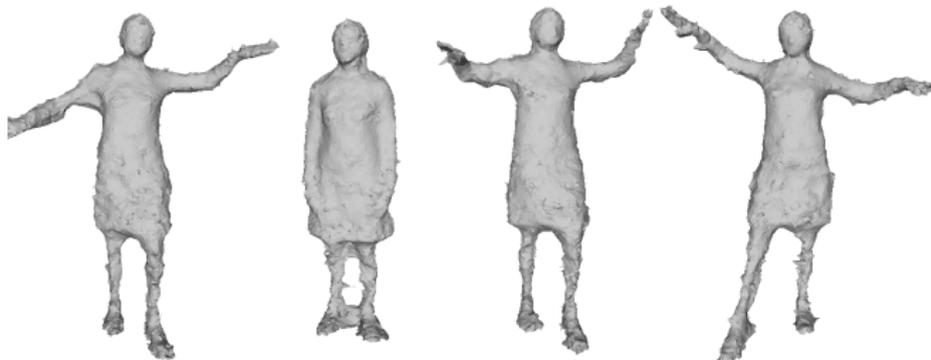
Marching cubes

Delaunay meshing

NB: same mesh size

Spatio-temporal visual hull using 4D Delaunay meshing

[Aganj et al 2007]



Approach

- ▶ Extend the previous algorithm to compute 4D visual hulls
⇒ 4D representation of the scene

Advantages over frame-by-frame computations

- ▶ Exploits time redundancy
 - ▶ Continuous representation, allowing spatio-temporal smoothing
 - ▶ Reduction of flickering artefacts in synthesized views
 - ▶ Handles naturally topological changes along time
- Requires an efficient implementation of DT in \mathbb{R}^4

Spatio-temporal multi-view oracle

A Delaunay **pentatope** is
part of the approx.
spatio-temporal visual hull



its circumcenter projects
inside the **time-interpolated**
silhouette in all views

Spatio-temporal multi-view oracle

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Accounts for spatio-temporal curvature
e.g. uniform motion \rightarrow coarser resolution

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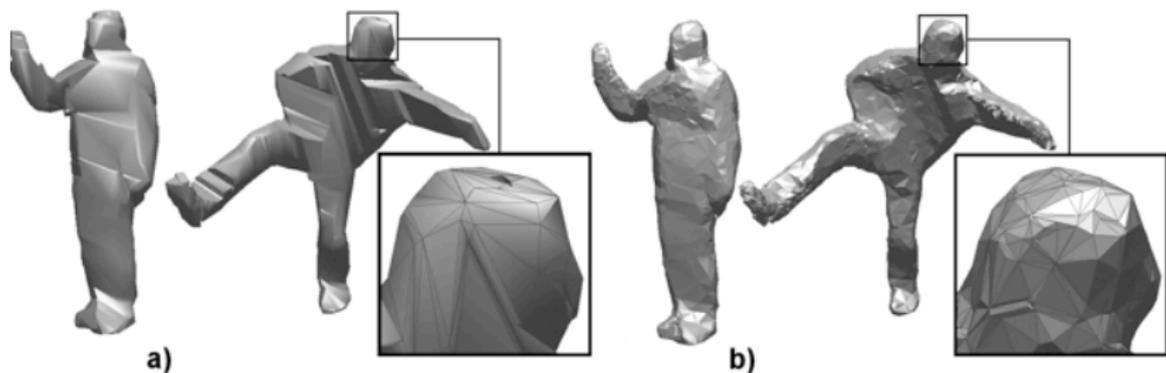
Refinement criterion = reprojection error

Accounts for spatio-temporal curvature
e.g. uniform motion \rightarrow coarser resolution

Computing 3D temporal slices

- ▶ The boundary B of STVH is a set of tetrahedra $\subset \mathbb{R}^4$
- ▶ March on the tet of B to compute the intersection of B with a hyperplane $t = \text{constant}$
- ▶ A 3-facet of $B \rightarrow \emptyset$, a triangle or a quad

Results on real data



Problem

To model moving surfaces undergoing large deformations and topology changes

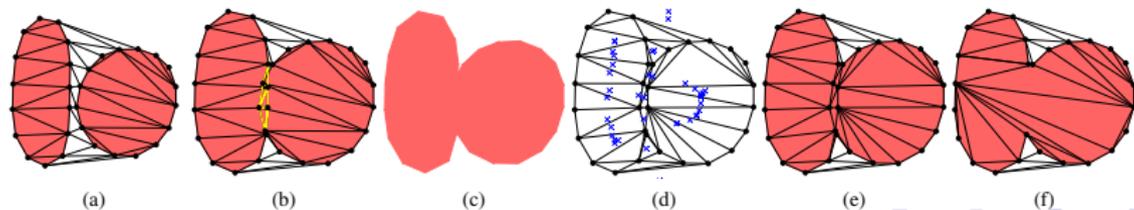
Our approach

- ▶ Represent the interface by a triangular mesh embedded in the restricted 3D DT of interface points
- ▶ Update the mesh at each time step by updating the RDT

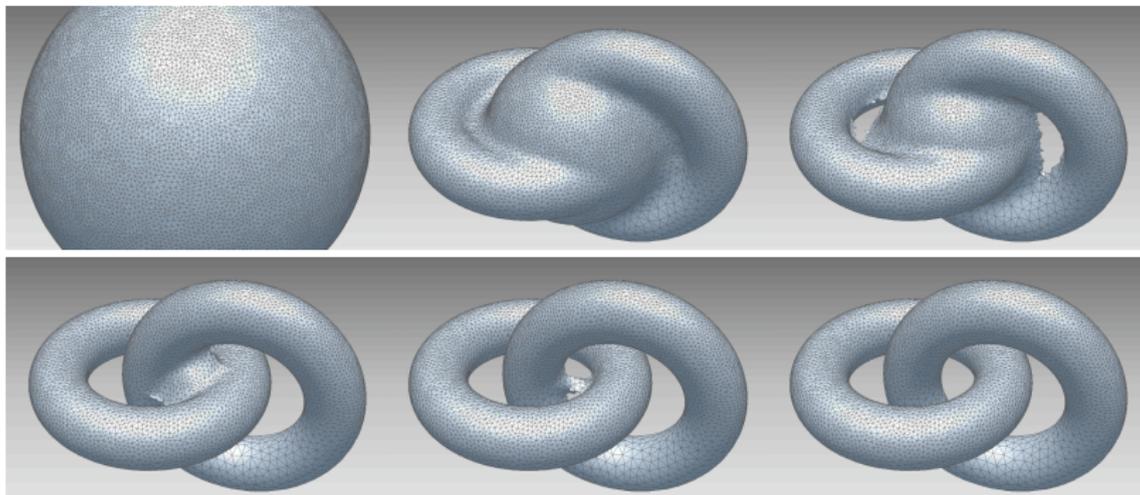
The algorithm at time step n

input: $\mathcal{P}_n = \text{sample}$, Ω_n , $D_n = \text{Del}_{|\Omega_n}(\mathcal{P}_n)$

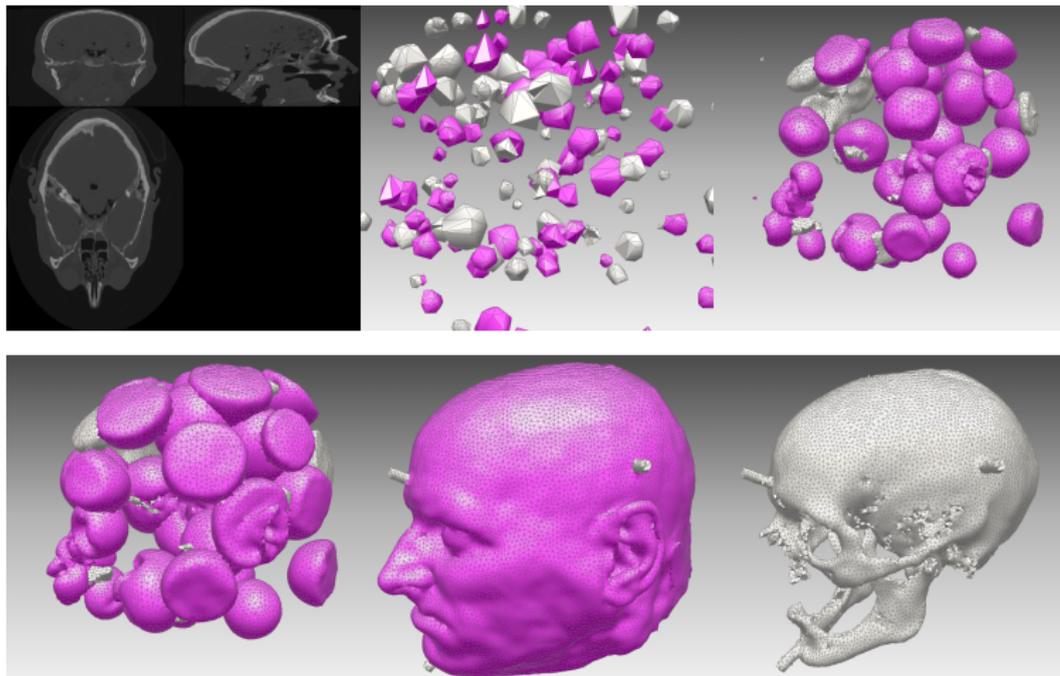
1. Move the points of \mathcal{P}_n
2. Adapt the sample resolution $\rightarrow \mathcal{P}_{n+1}$
 - 2.1 replace a too short edge of D_n by its midpoint
 - 2.2 add the midpoint of a too long edge
3. Deal with topology changes
 - 3.1 discard tetrahedra that have been inverted
$$\Omega_{n+1} = \bigcup \{ \tilde{\tau} \mid \tau \in D_n, \text{orient}(\tilde{\tau}) \times \text{orient}(\tau) < 0 \}$$
 - 3.2 $D_{n+1} = \text{Del}_{|\Omega_{n+1}}(\mathcal{P}_{n+1})$
 - 3.3 remove the vertices whose incident simplices all share the same label



A sphere deforming into a torus



Application to image segmentation



Collaboration with J-P. Pons (CERTIS)

Meshing 3D domains by Delaunay refinement

The surface mesher

- ▶ inserts points on the surface S
- ▶ triangulates the **ambient** space and extracts the Delaunay triangulation restricted to S
- ▶ controls the shape of the triangles of $\text{Del}_S(\mathcal{P})$

Meshing 3D domains by Delaunay refinement

The surface mesher

- ▶ inserts points on the surface S
- ▶ triangulates the **ambient** space and extracts the Delaunay triangulation restricted to S
- ▶ controls the shape of the triangles of $\text{Del}_S(\mathcal{P})$

Hence

- ▶ it can triangulate the domain O bounded by S at no additional cost
- ▶ but does not provide control on the shape of the tetrahedra inside O

3-d mesh refinement algorithm

1. Run the surface meshing algorithm
2. Insert points inside O to remove the bad elements of $\text{Del}_S(\mathcal{P})$ and $\text{Del}_O(\mathcal{P})$

Sizing field

$\psi(x)$ defined over O

Basic procedures

`refine_face(f)` : insert c_f , the center of the surface
Delaunay ball circumscribing f

`refine_tet(t)` : insert c_t , the center of the ball
circumscribing t

Sizing field

$\psi(x)$ defined over O

Basic procedures

`refine_face(f)` : insert c_f , the center of the surface
Delaunay ball circumscribing f

`refine_tet(t)` : insert c_t , the center of the ball
circumscribing t

Bad elements

bad facet f : $r_f > \alpha\psi(c_f)$
or f has a vertex $\notin S$

bad tet. t : tetrahedron whose circumscribing ball has
radius $r_t > \psi(c_t)$ or a radius-edge ratio $> \rho$

Step 2 : Apply the following rules in order

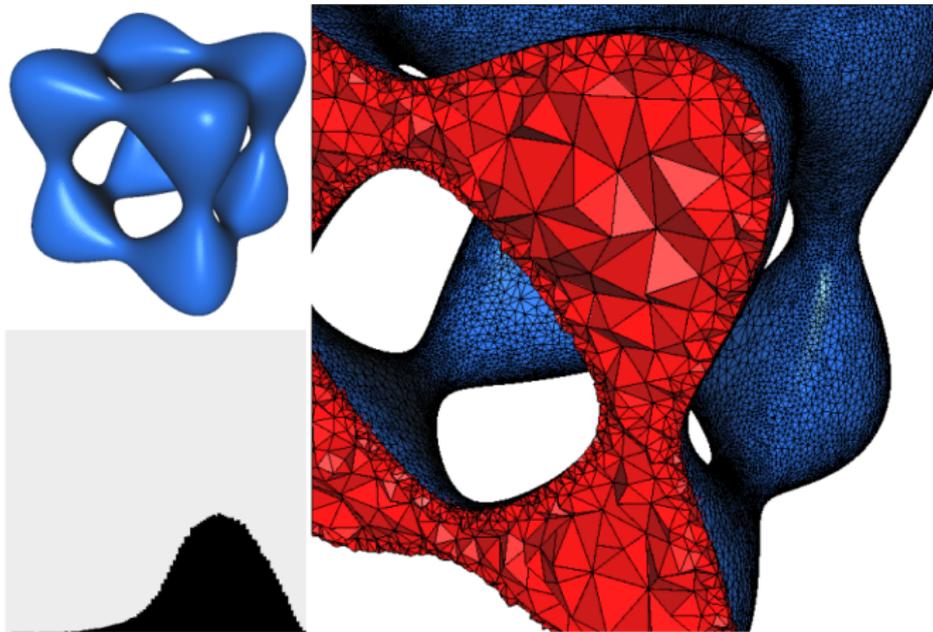
1. if $f \in \text{Del}_S(\mathcal{P})$ is a bad facet, `refine_face(f)`
2. if $t \in \text{Del}_O(\mathcal{P})$ is a bad tetrahedron,
 - 2.1 if c_t is included in a surface Delaunay ball B_f ,
`refine_face(f)`
 - 2.2 else `refine_tet(t)`

Step 2 : Apply the following rules in order

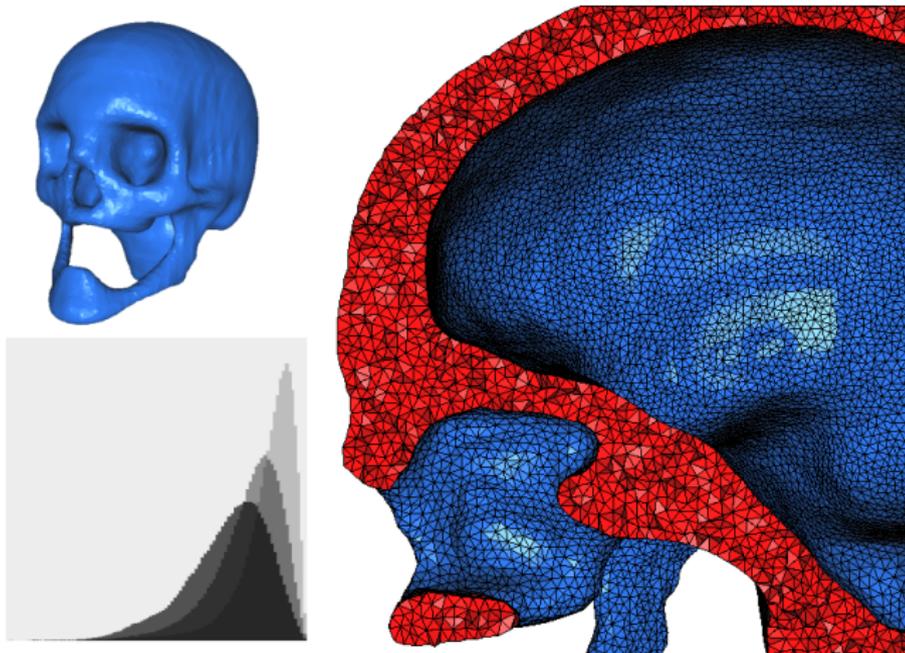
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 - 2.1 if c_t is included in a surface Delaunay ball B_f ,
`refine_face(f)`
 - 2.2 else `refine_tet(t)`

Properties

1. For appropriate α and ρ , the algorithm terminates
2. $\text{Del}_S(\mathcal{P}) = \text{Del}_S(\mathcal{P} \cap S)$ (cf. def of bad facet)
3. hence $\text{Del}_S(\mathcal{P})$ is a 2-triangulation isotopic to S
 $\text{Del}_O(\mathcal{P})$ is a 3-triangulation isotopic to O



Non uniform mesh



Uniform mesh

33,012 initial vertices, $2,471 + 53,762$ new vertices
20s (Pentium IV, 1.7 GHz)

Multibody mesh generation from segmented images

input : a segmented 3D image (each voxel has a label)

label of a tetrahedron: label of its circumcenter

boundary facet : dual to a Voronoi edge whose endpoints have two different labels

Multibody mesh generation from segmented images

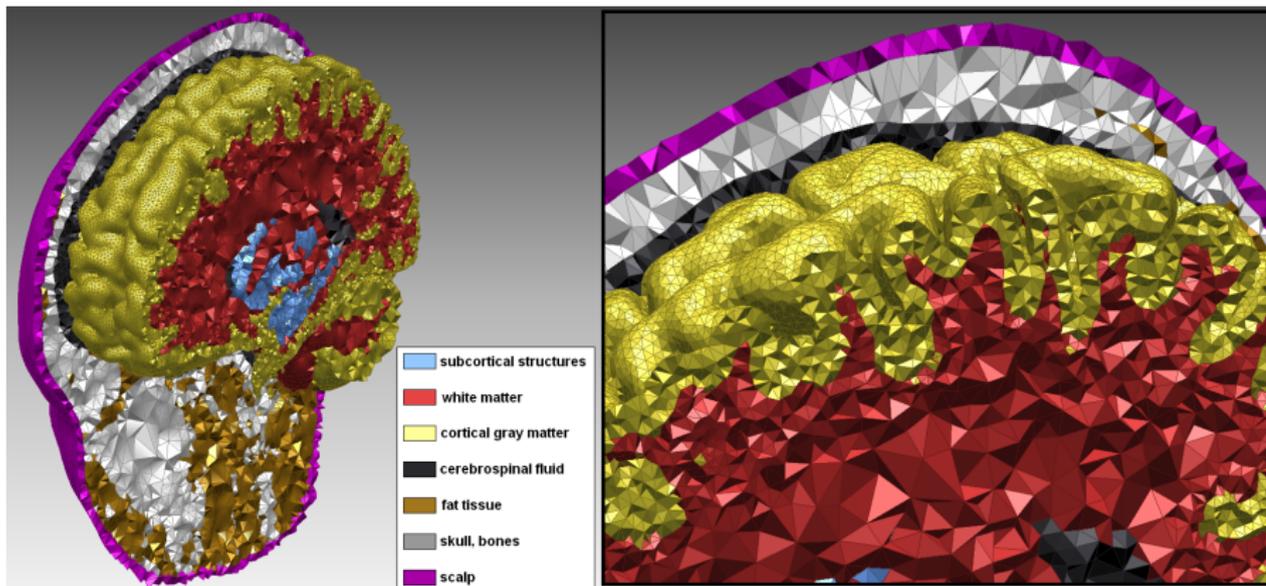
input : a segmented 3D image (each voxel has a label)

label of a tetrahedron: label of its circumcenter

boundary facet : dual to a Voronoi edge whose endpoints have two different labels

- ▶ We mesh simultaneously the various tissues using Delaunay refinement
- ▶ The boundary facets produce a good approximation of the interfaces
 - all boundary surfaces are water tight and don't intersect each other
- ▶ The tetrahedra of a given label produce a good approximation of the associated tissue

Multibody mesh generation from segmented images



Tissue-dependent resolution

77 tissues, 389K vertices, 536K boundary facets, 536K tets
23 mn

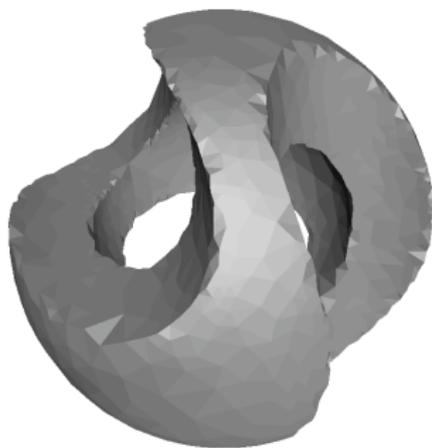
Collaboration with CERTIS



Zigzagging effect along sharp features

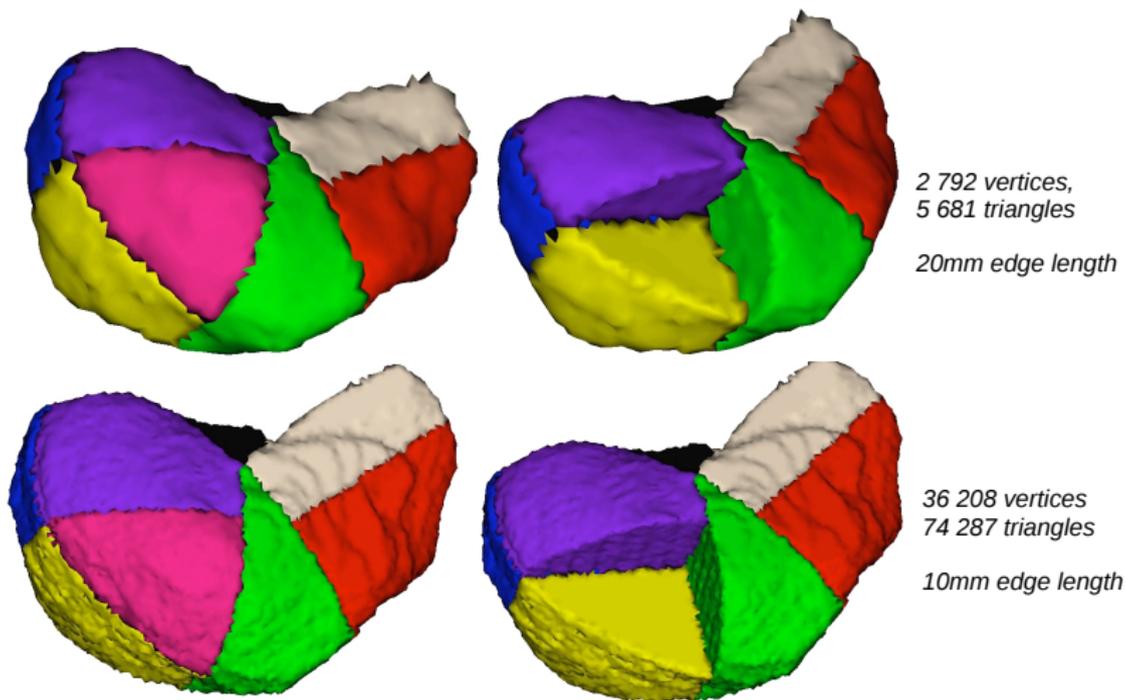


Input domain



Output mesh

Zigzagging effect along 1-junctions between 3 or more tissues

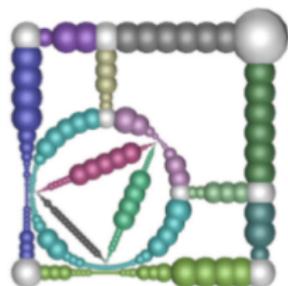
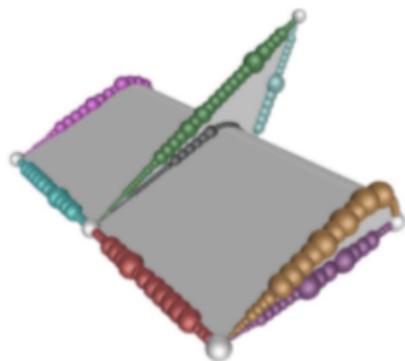


Meshing 3D domains with piecewise smooth boundaries

[Dey & Levine]

Protecting balls

- ▶ centered on the sharp features F of S
- ▶ B cannot contain the center of $B' \neq B$
- ▶ the balls cover F
- ▶ no 3 balls intersect

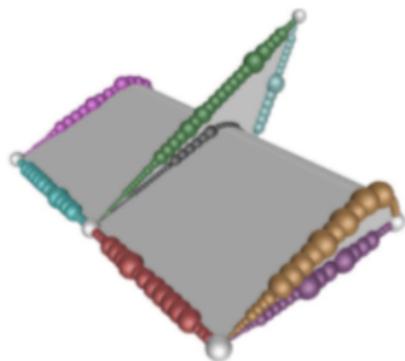


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[Dey & Levine]

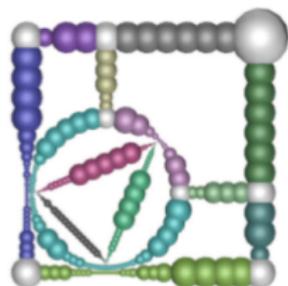
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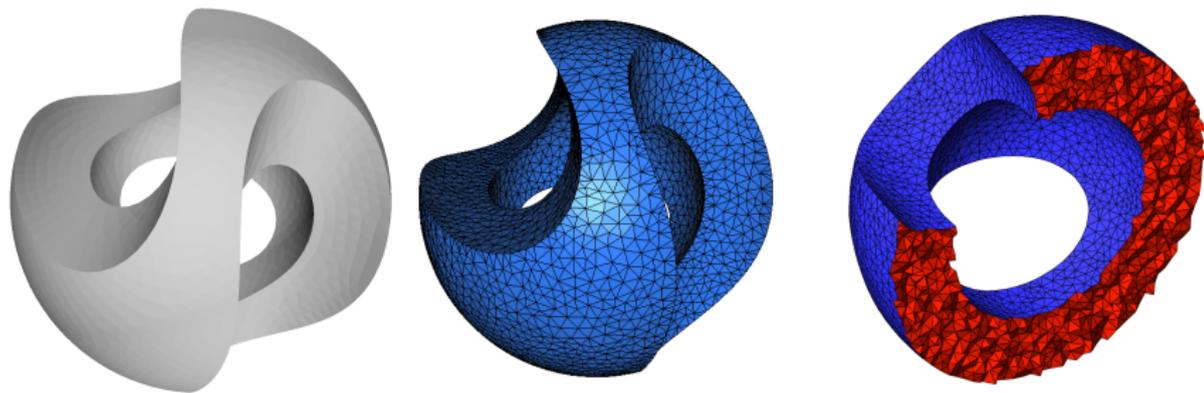


Algorithm

- ▶ Use the **weighted** DT
- ▶ Insert the protecting balls first
- ▶ Insert **unweighted** points inside O as usual



Meshing 3D domains with piecewise smooth boundaries



6 052 vertices
37 106 cells
8,87° smallest dihedral angle

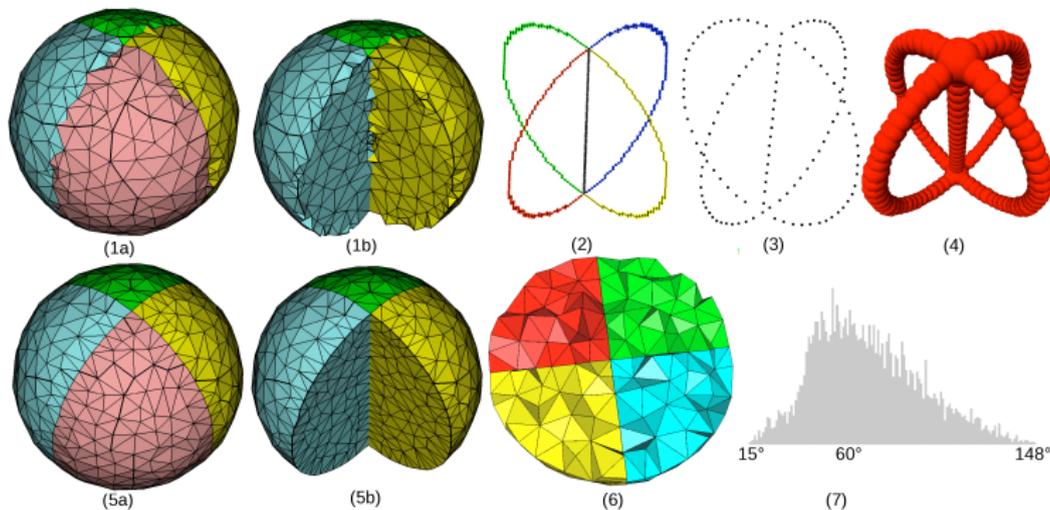


Figure 2: (1) Delaunay refinement 3D mesh. (2) Multi-material junctions: five 1-junctions and two 0-junctions. (3) Sampled points on junctions. (4) Protecting balls. (5) Feature preserving Delaunay refinement 3D mesh. (6) A cut of the tetrahedral mesh. (7) Histogram of the dihedral angles.

[Boltcheva et al. 2009]

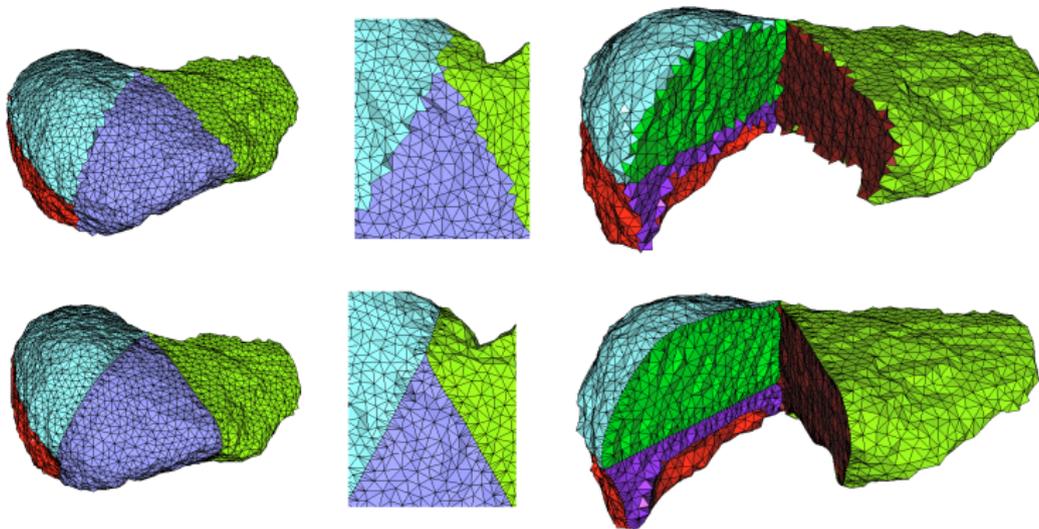
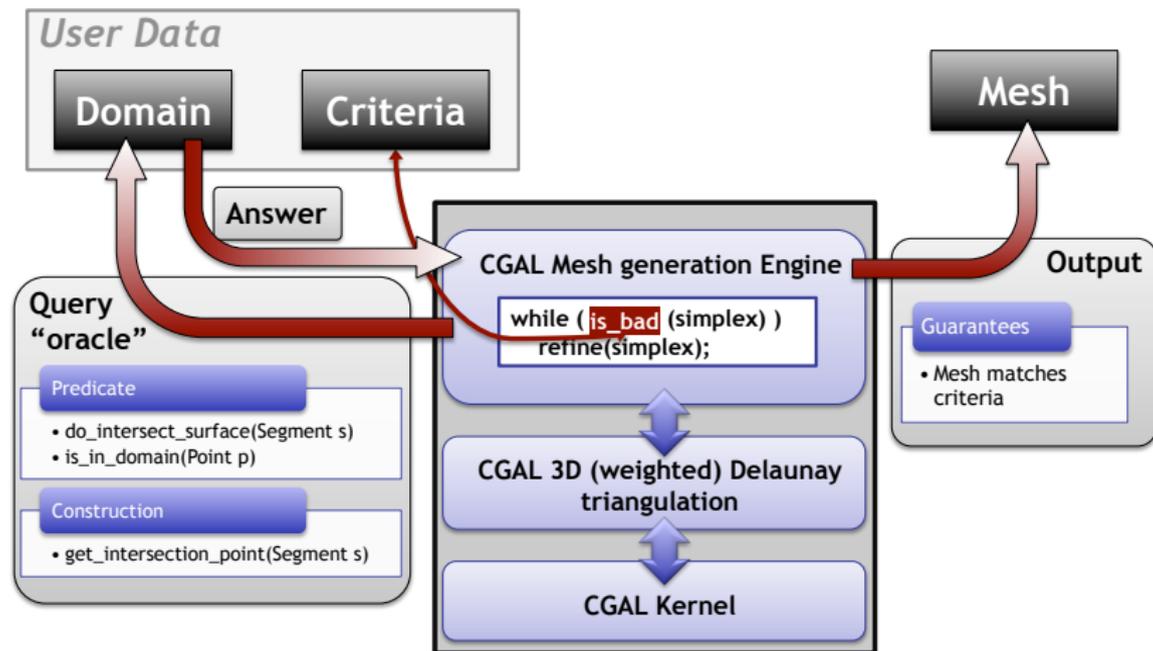
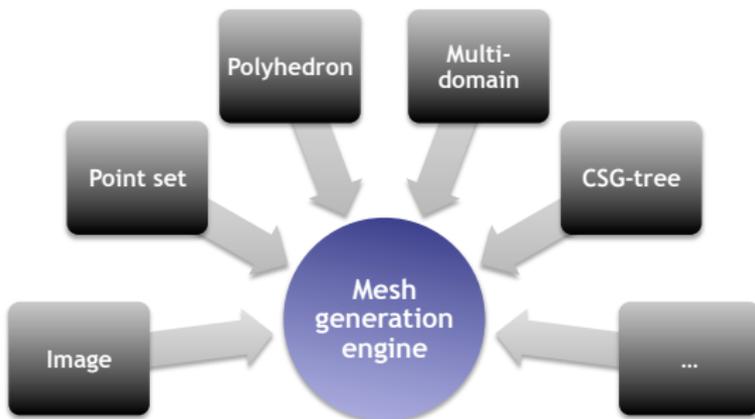


Figure 7: Meshes generated from a segmented liver image representing 4 anatomical liver regions. The first row shows meshes obtained with the usual Delaunay refinement algorithm. The second row shows meshes generated with our feature preserving extension. The 3rd column shows some internal interfaces between the anatomical regions.

[Boltcheva et al. 2009]



- core mesh generation algorithm independent from the input domain representation



Acknowledgments

Students and colleagues

S. Oudot	Surface mesh generation [2005]
L. Rineau	3D domains mesh generation [2007]
C. Wormser	Anisotropic mesh generation [2008]
J. Tournois	Mesh optimization [2009]
J-P. Pons	Applications in computer vision
D. Boltcheva	Applications in medical imaging
N. Salman	Applications to surface reconstruction
P. Alliez, L. Rineau, S. Tayeb, M. Yvinec	CGAL-mesh

Acknowledgments

Projects

The CGAL library : <http://www.cgal.org>

IST Programme of the EU :

- ▶ ECG Project (Effective Computational Geometry for Curves and Surfaces)
<http://www-sop.inria.fr/prisme/ecg/>
- ▶ ACS Project (Algorithms for complex shapes)
<http://acs.cs.rug.nl/>

ADT CGAL-mesh